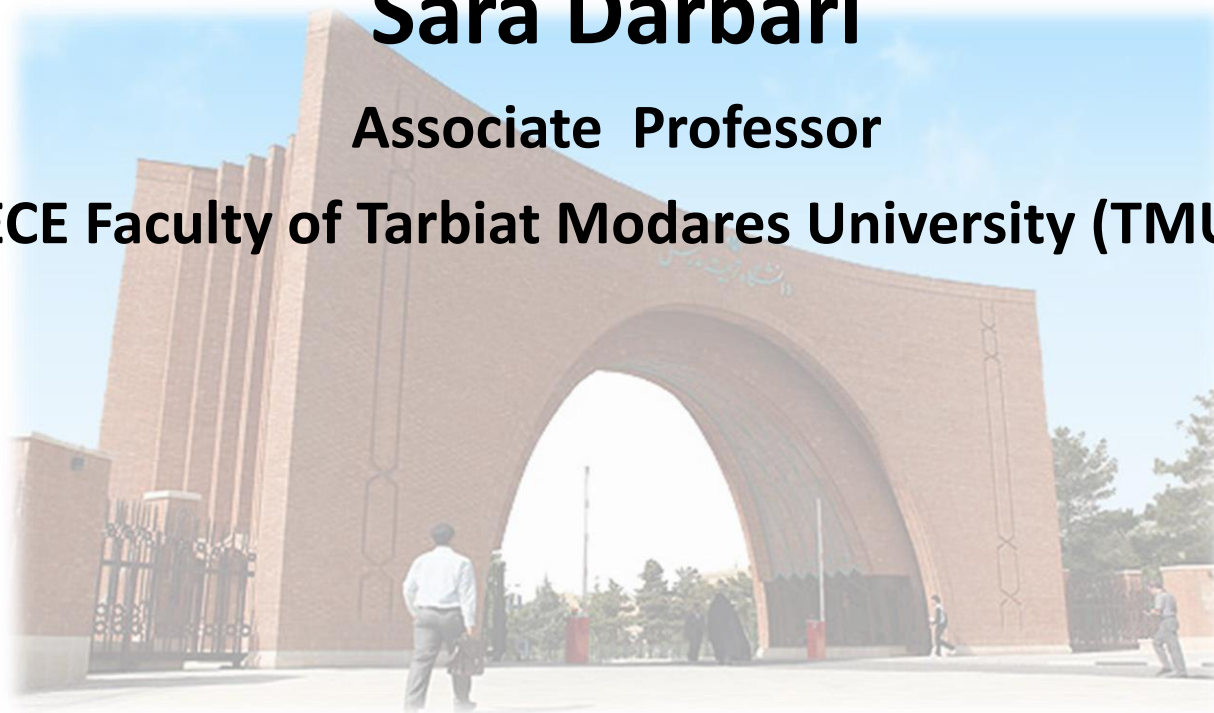


Manipulation of bio-particles by surface acoustic waves (SAWs)

Sara Darbari

Associate Professor

ECE Faculty of Tarbiat Modares University (TMU)



- The Faculty of Electrical and Computer Engineering (ECE), one of the oldest Faculties in TMU.



Nanosensors and Detectors Lab. (NSDL) and my research group

NSDL, founded in 2017



My research group



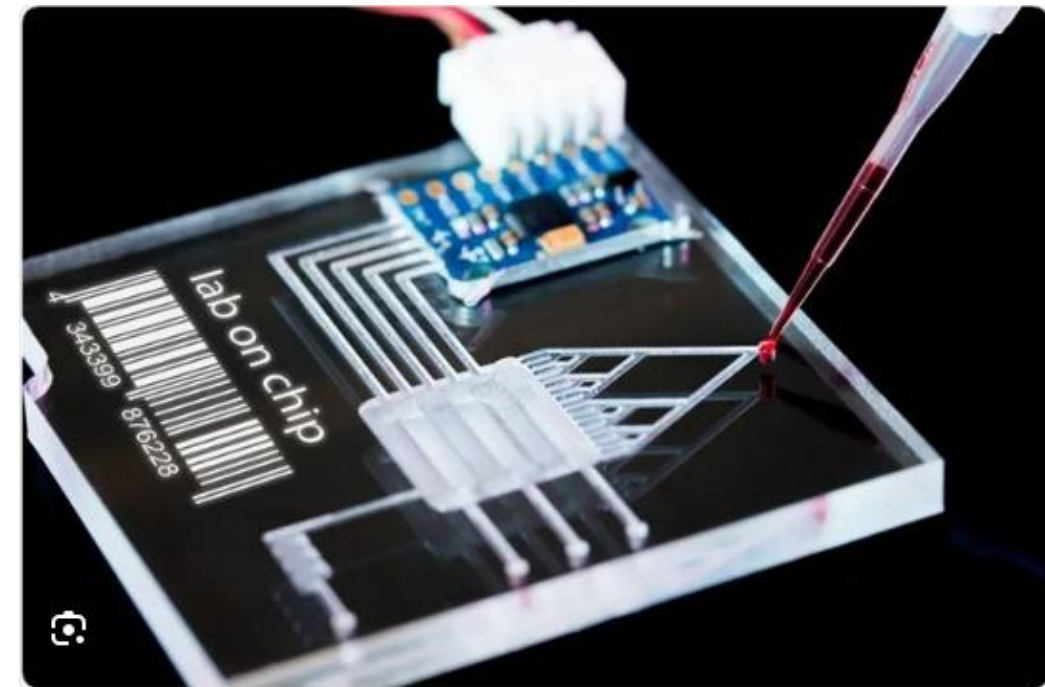
Introduction

Surface acoustic waves (SAW) for particle manipulation

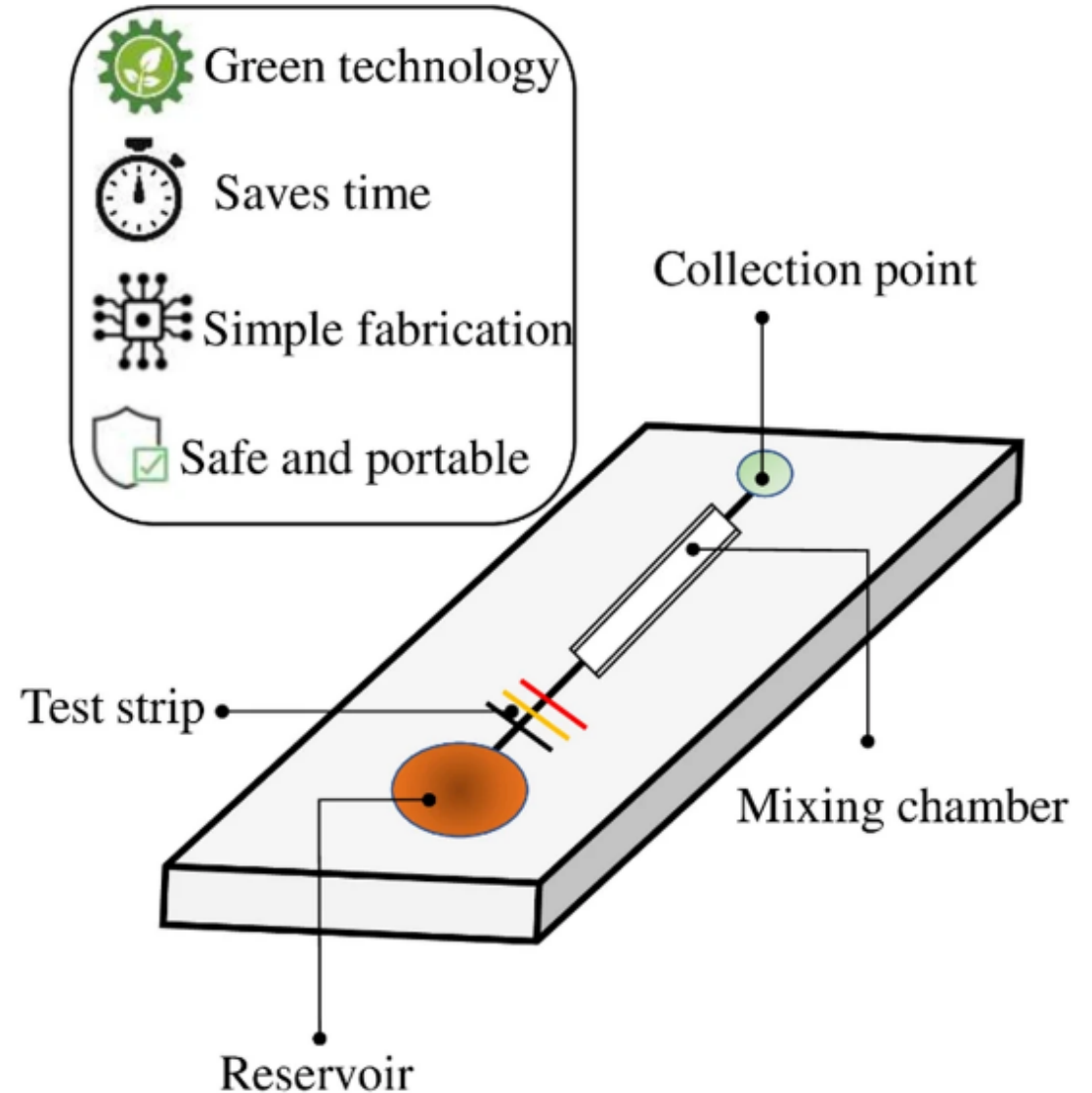
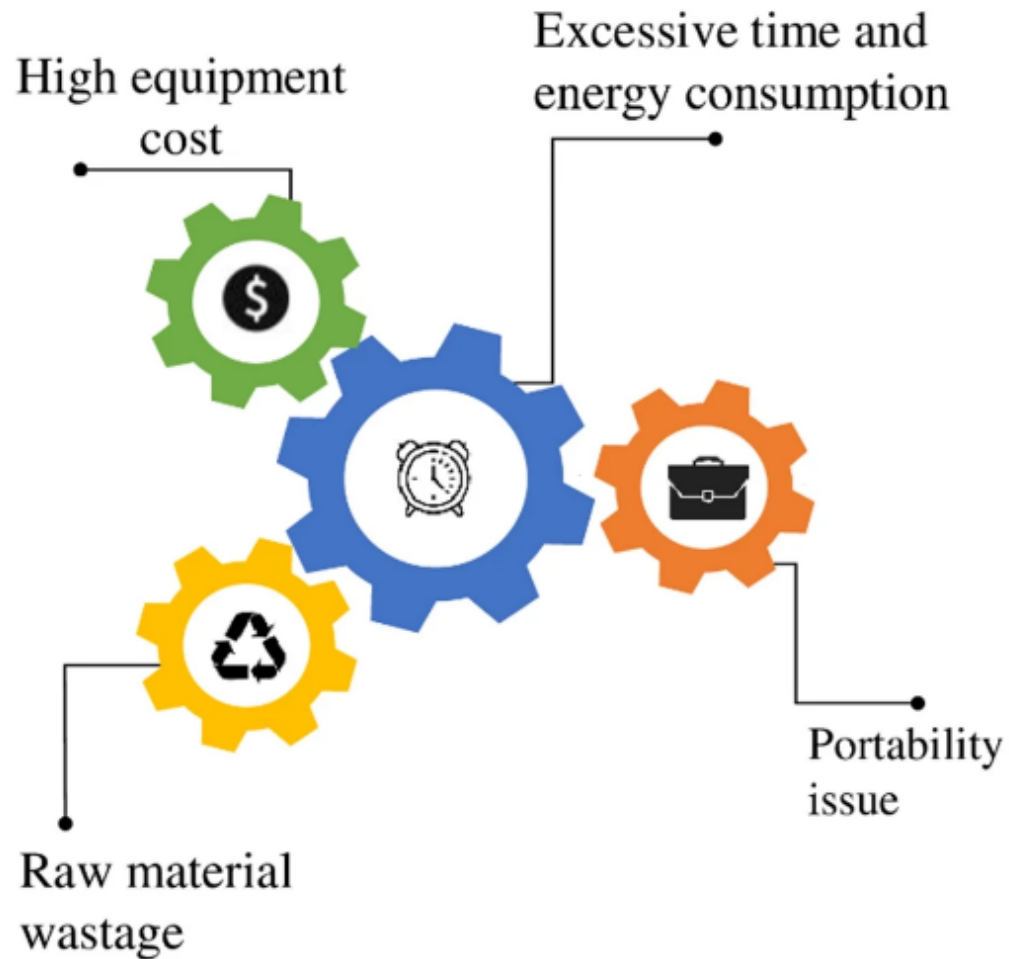
- Introduction to SAW-based tweezers
- Convex-Concave IDT electrodes for efficient separation of WBCs
- Surface coupled locally resonant modes
- Reinforced and localized SAW-based tweezers
- SAW-in-capillary separation of highly motile sperm
- Acoustic treatment in freezing/thawing of sperm
- SAW-biosensor for detection of Cardiac Troponin I

Microfluidics and Lab-on-chip

- Microfluidic systems are non-turbulent, highly ordered, fluid flow systems that are typically used in controlled biological experiments.
- The size of microfluidic devices is about a few hundred microns.
- The ability to put an entire laboratory procedure into a simple microsystem has given this technology the name “lab on a chip”
- Within the microfluidic chip, fluids are mixed, separated or directed, as the experiment requires.
- The outcome is an automated multiplexed system which can achieve high throughput.



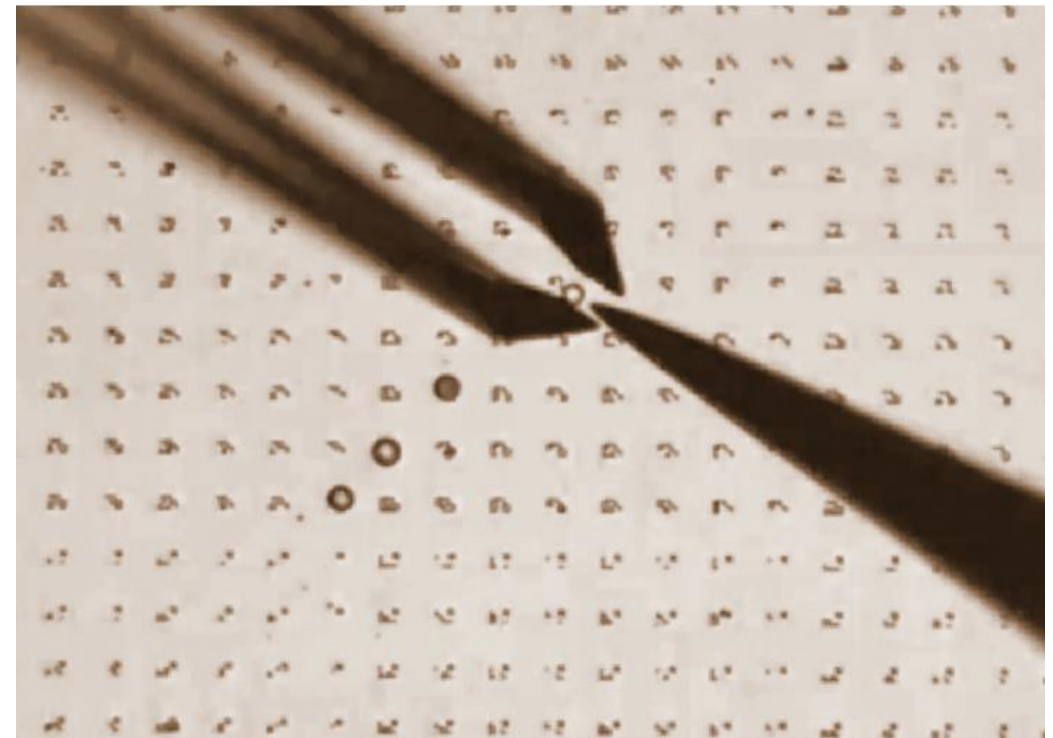
Clinical analysis versus Lab-on-chip



Manipulation of target particles

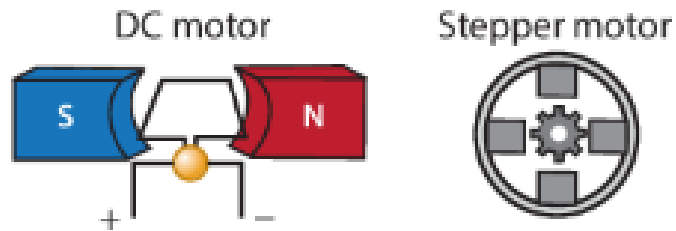


Reducing the
particle size

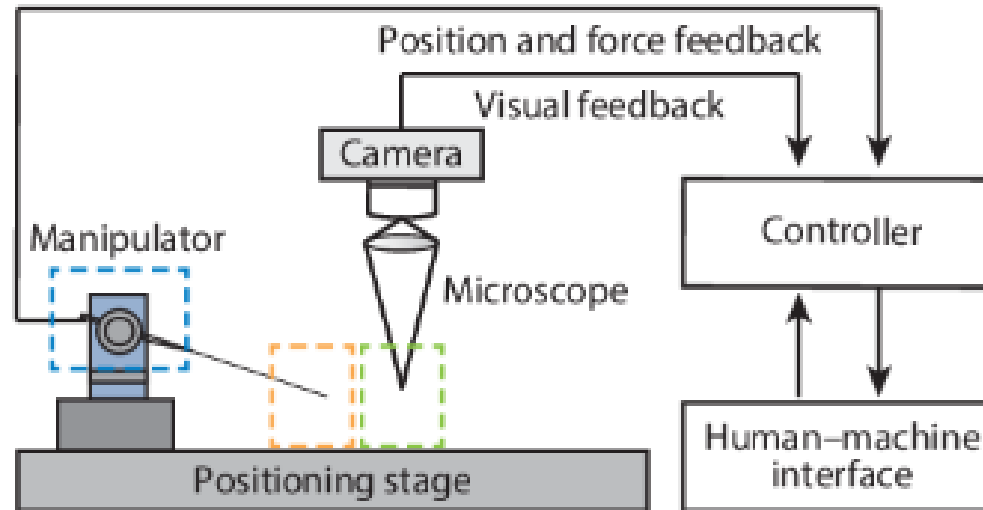
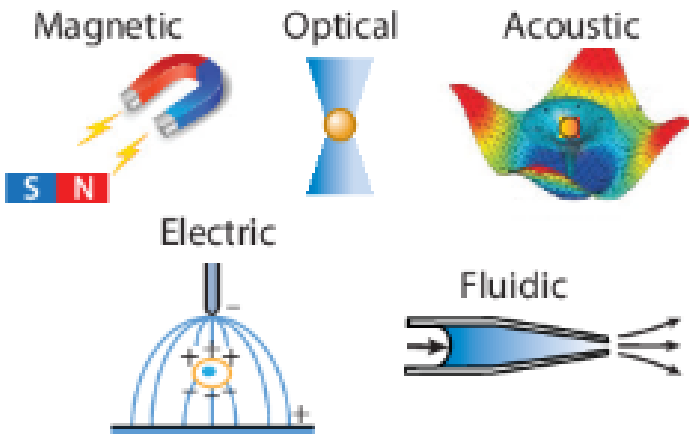


Manipulation of target micro-particles

Actuation using micromanipulators



Actuation using remote physical fields

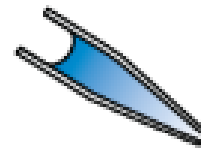


End effectors

Microgripper



Micropipette



Cantilever



Manipulated objects

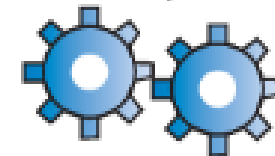
Organelle



Single cell



Micropart



Small organism



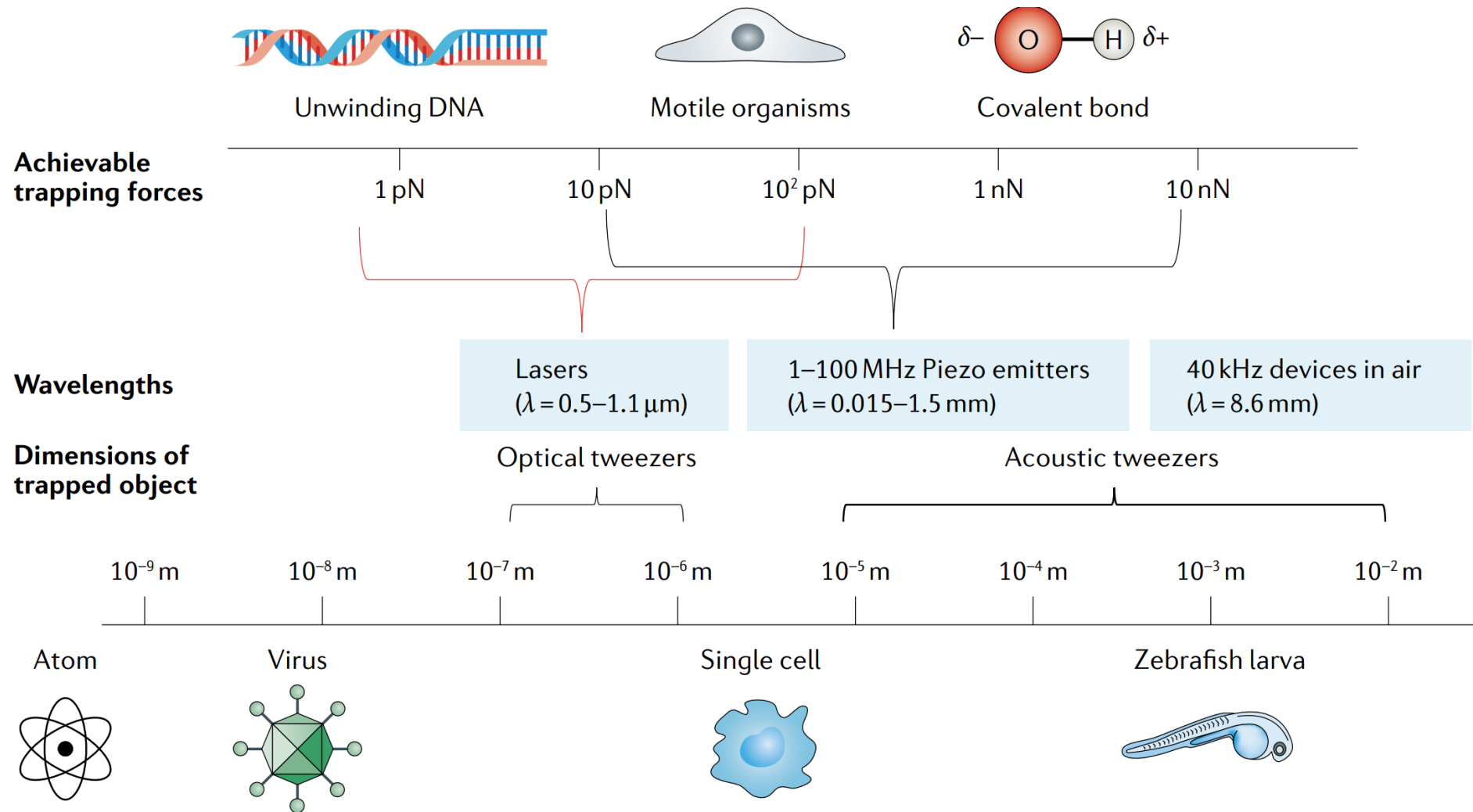
100 nm

1 μ m

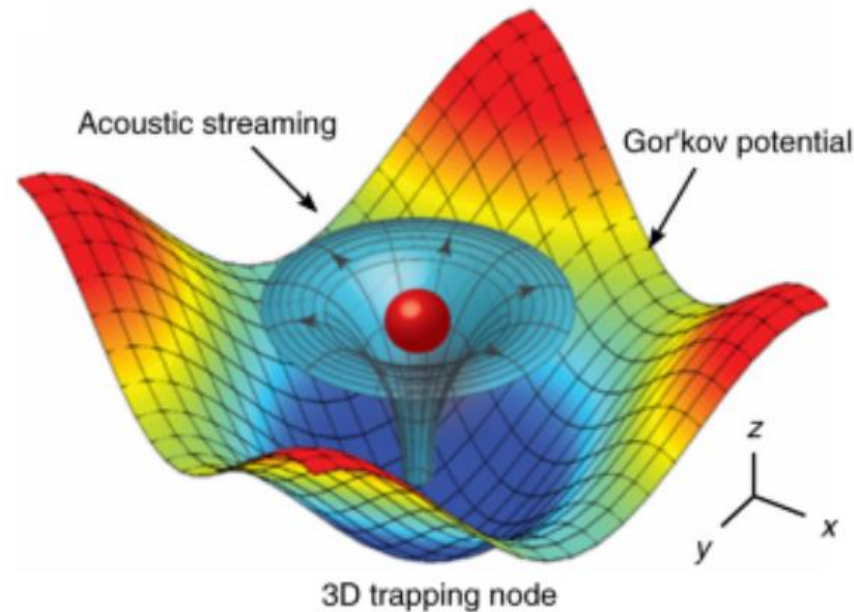
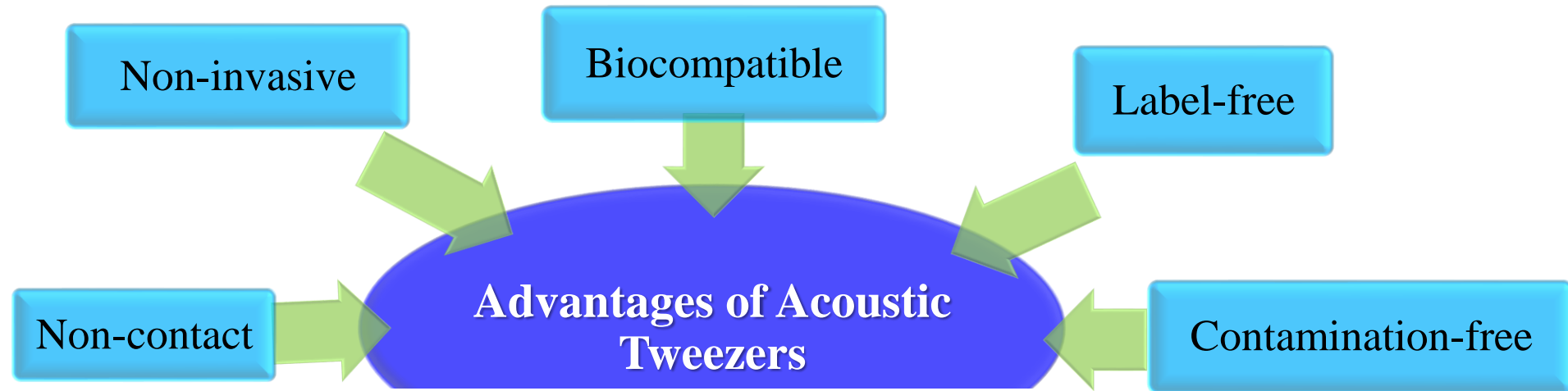
100 μ m

1 mm

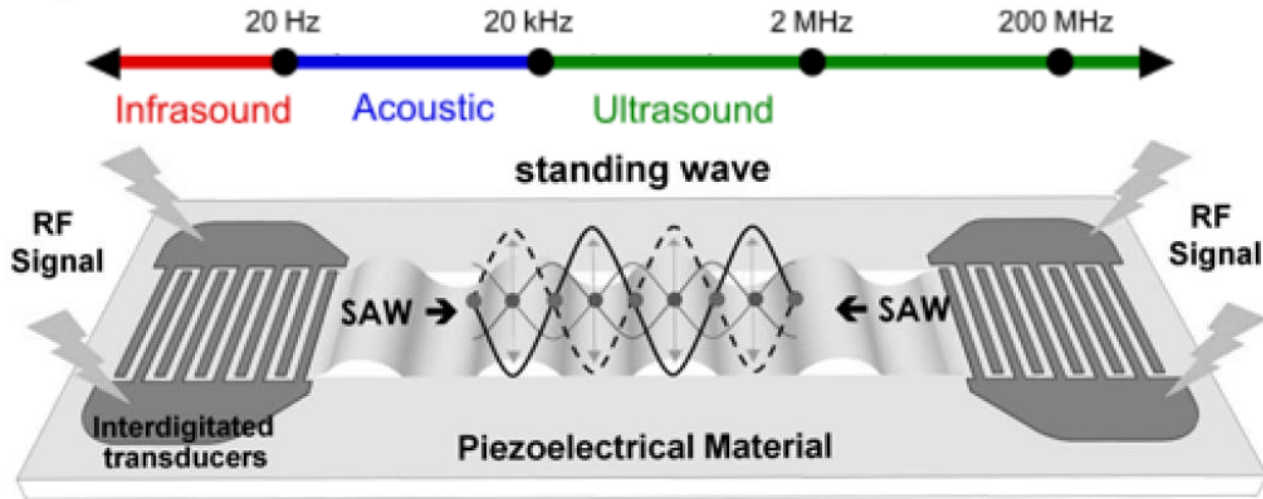
Acoustic/optical manipulation of micro-particles



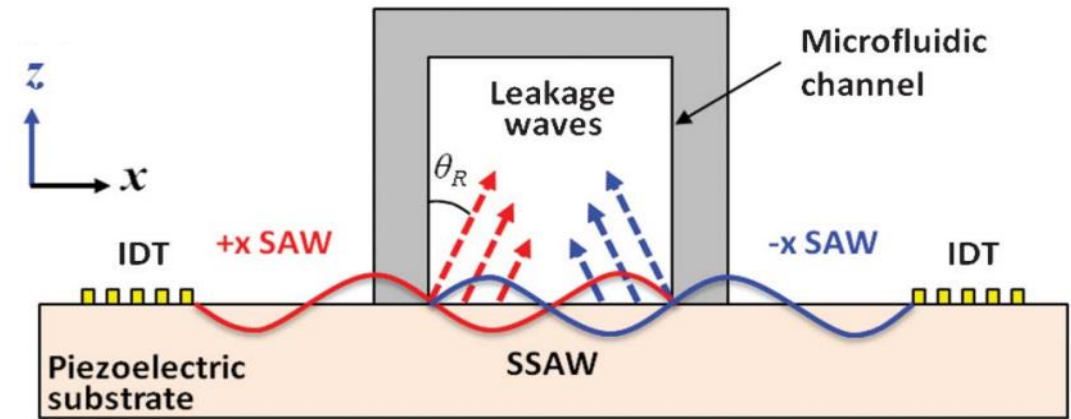
Advantages of Acoustic Tweezers



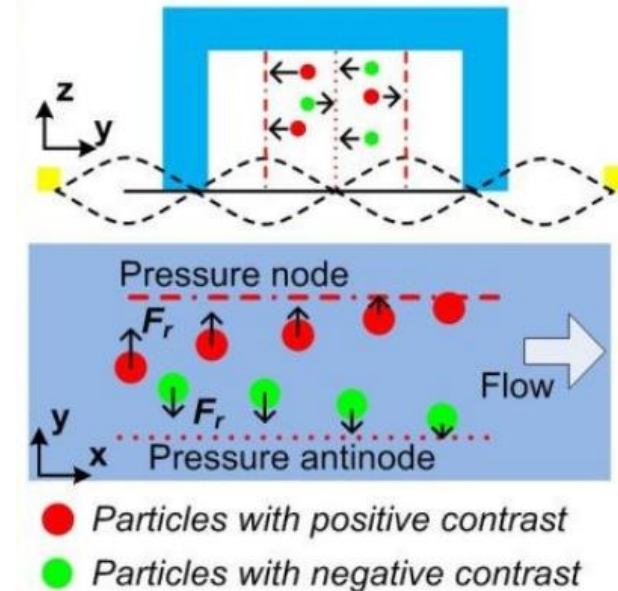
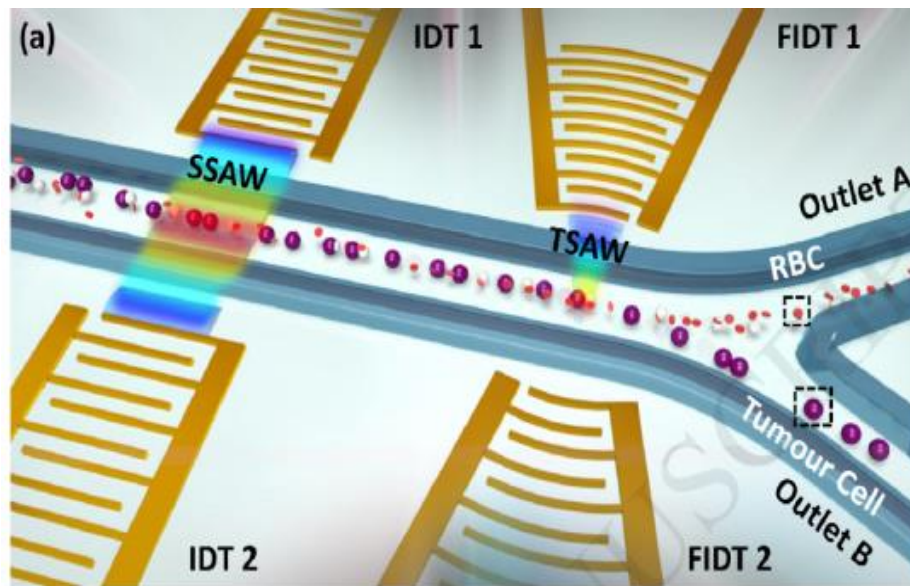
SAW-based manipulation of micro-particles



J. Nam, et al., (2011), Korea- Aust Rheol. J.

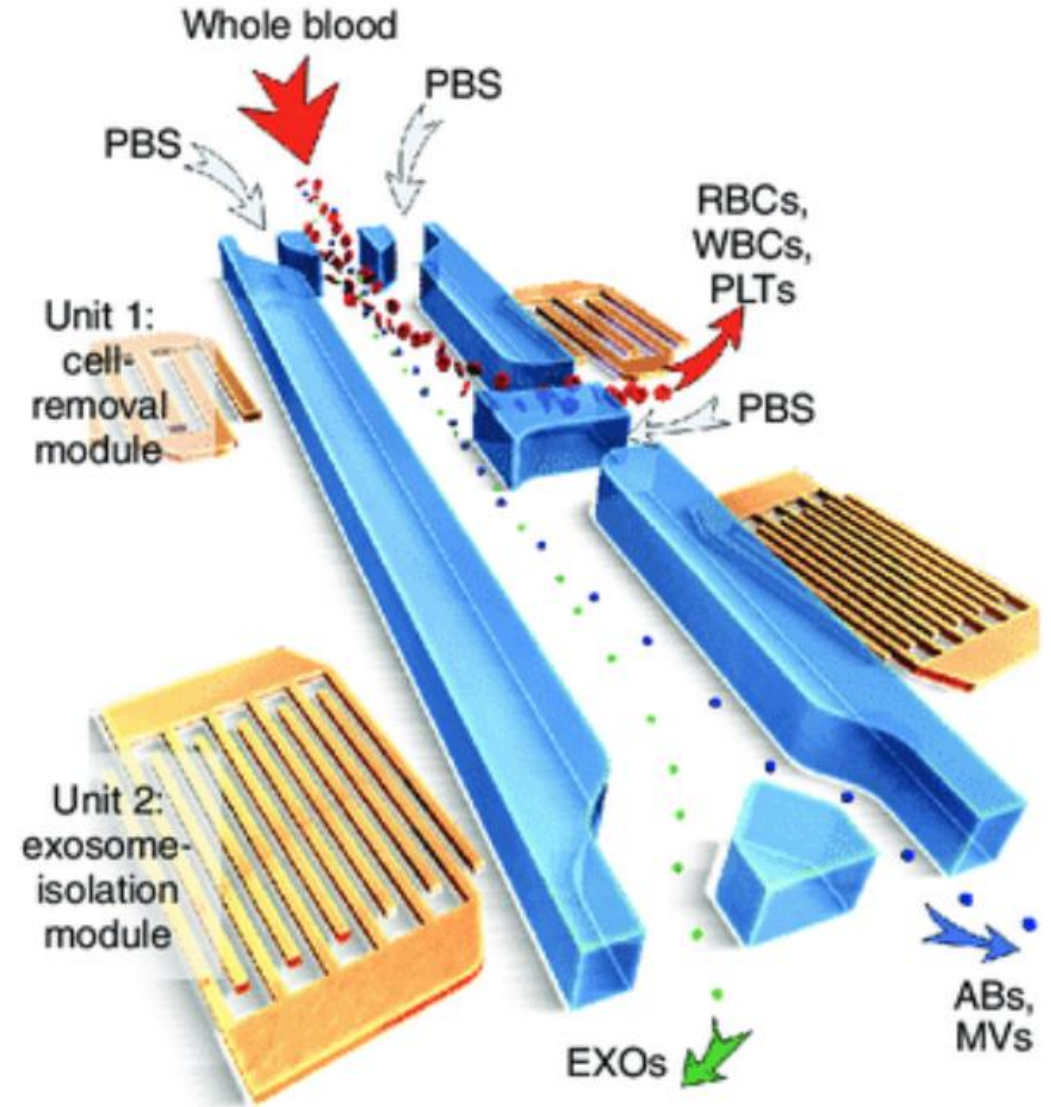
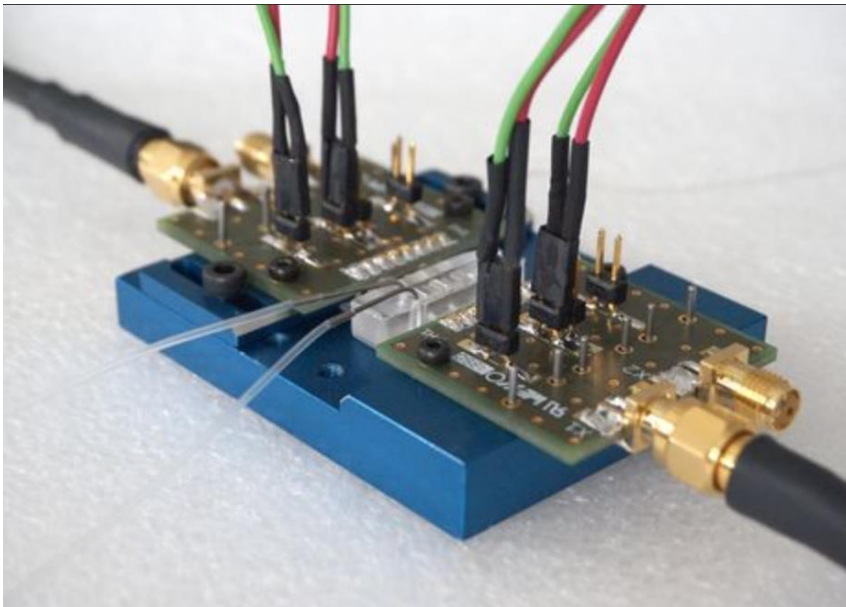
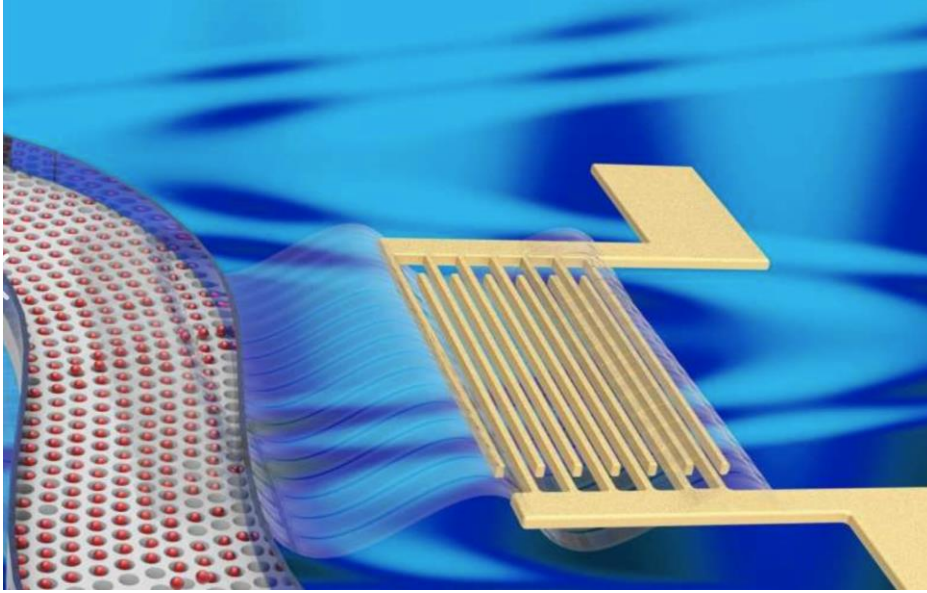


X. Ding, *Lab Chip*, 2013

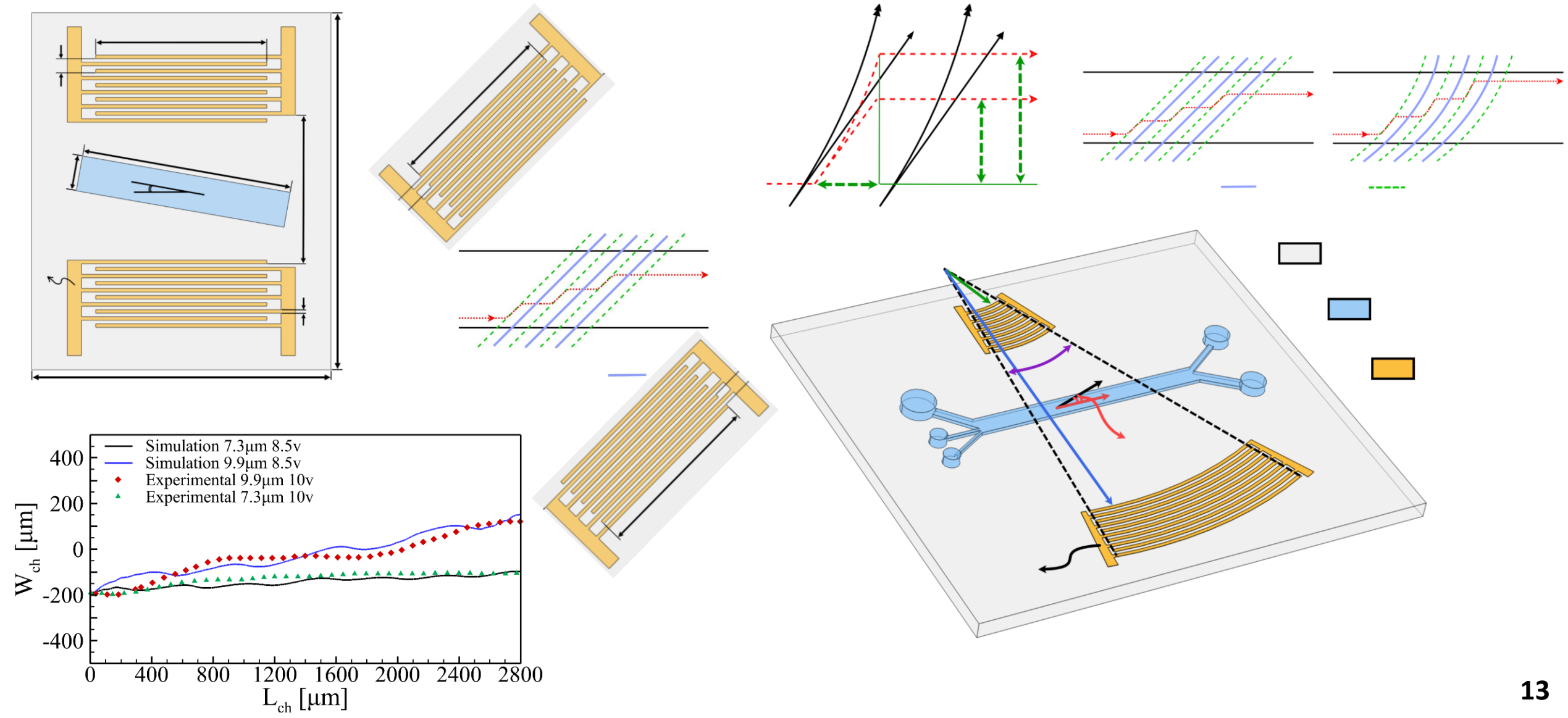


M. Wu et al., *Lab Chip*, 2019

Acoustofluidic: Acoustic Manipulation in Microfluidics

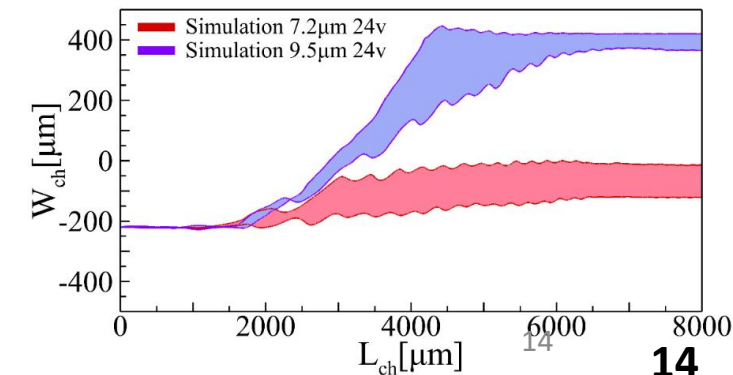
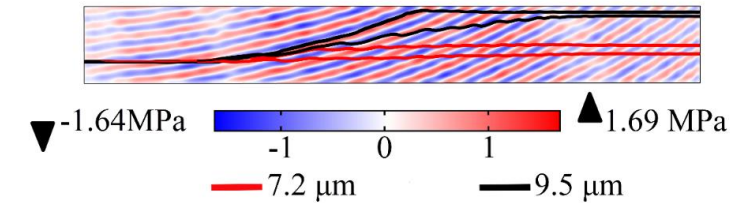
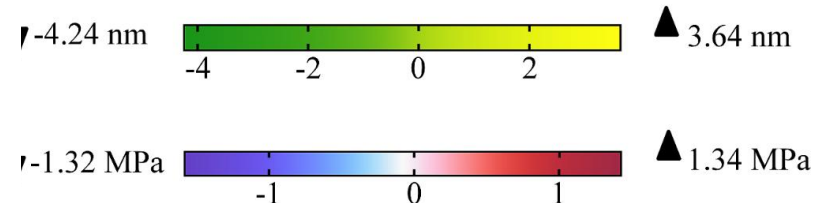
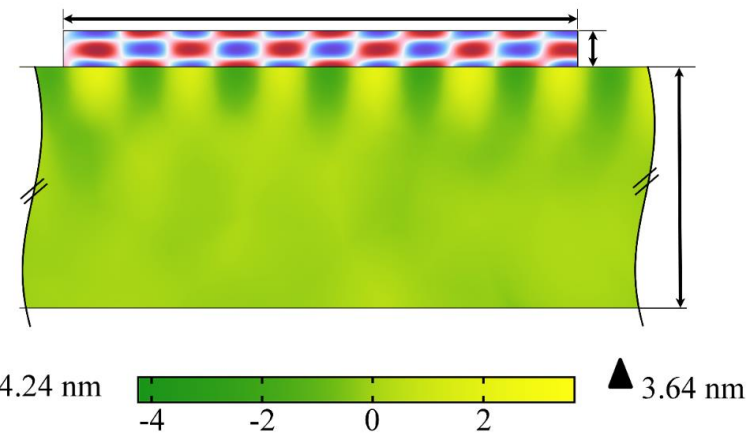
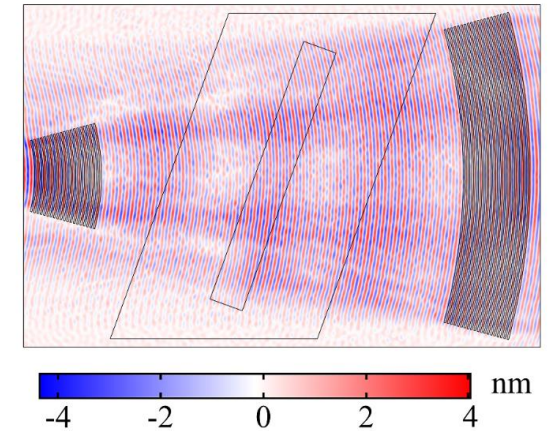
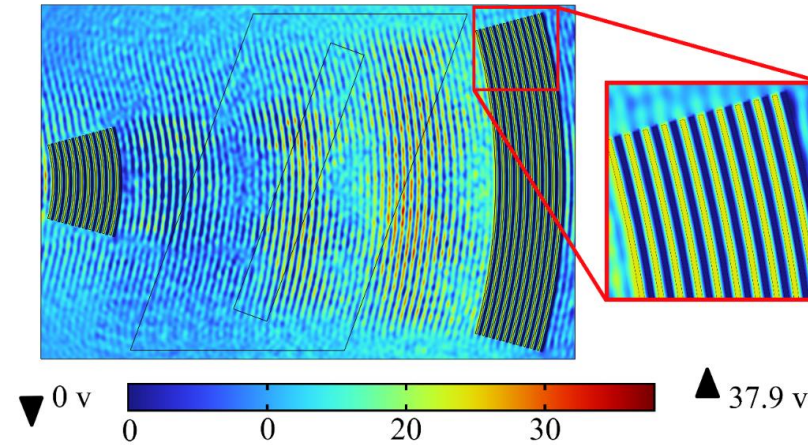
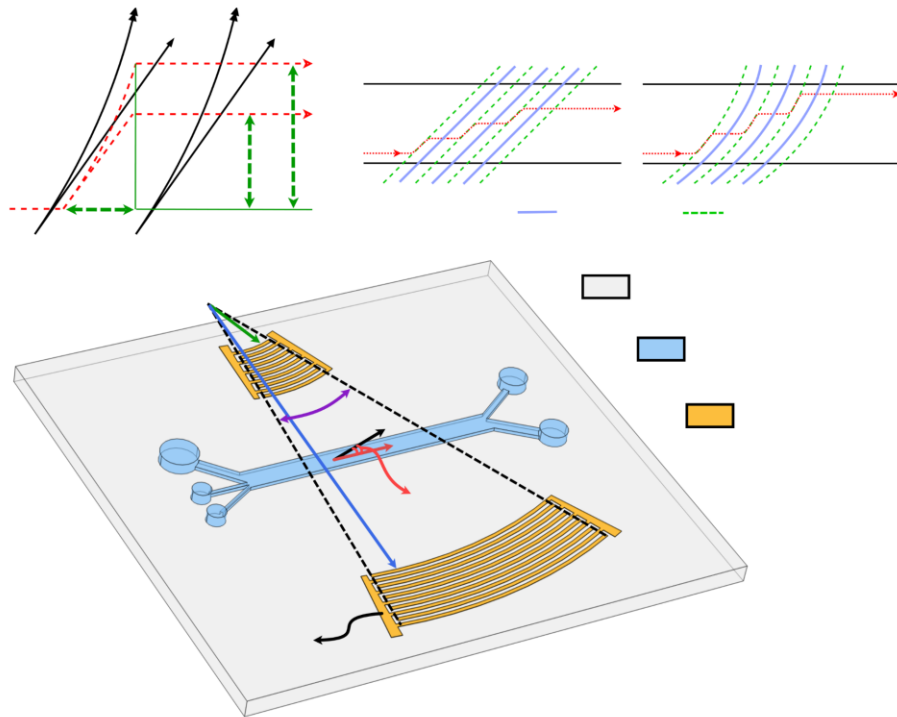


SAW-based separation of WBCs by concave/convex IDTs



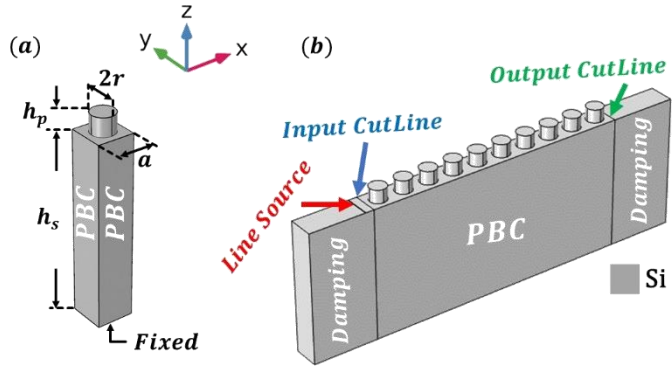
SAW-based separation of WBCs by concave/convex IDTs

Separating lymphocytes from other WBCs, as a demonstration of separating close-sized bio-particles.

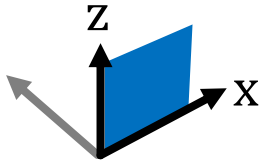


15

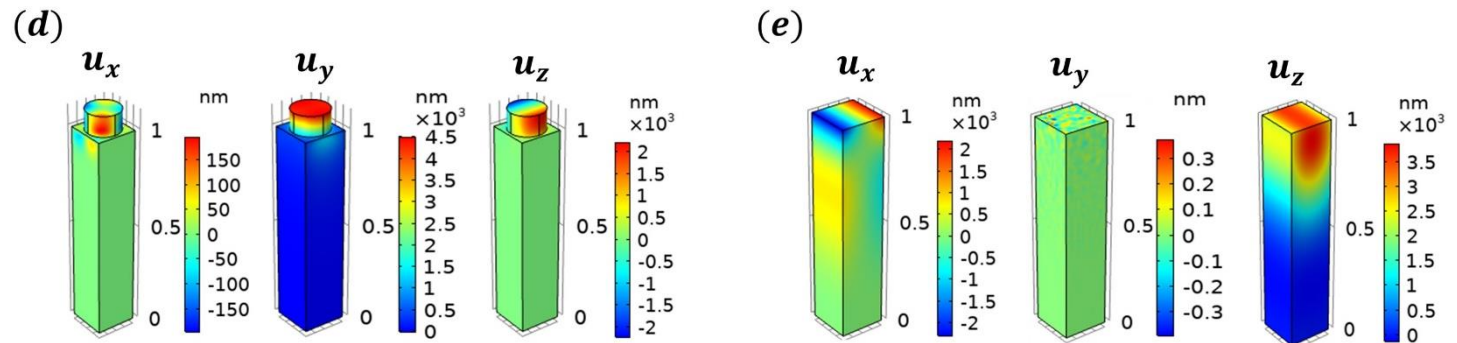
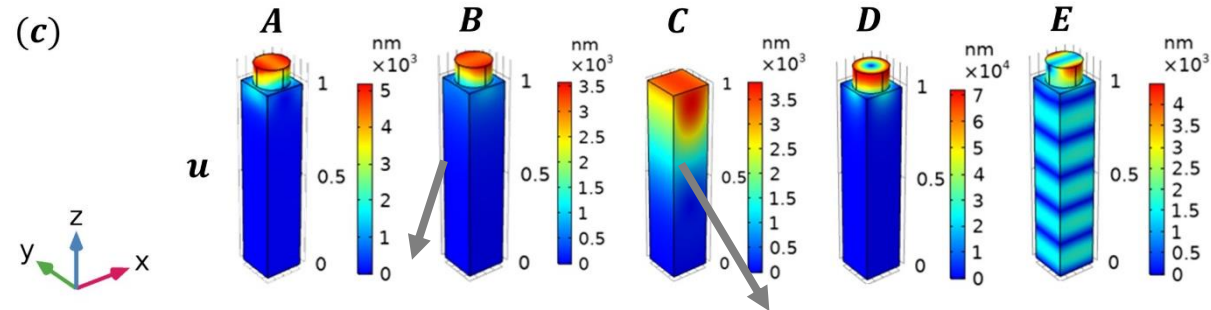
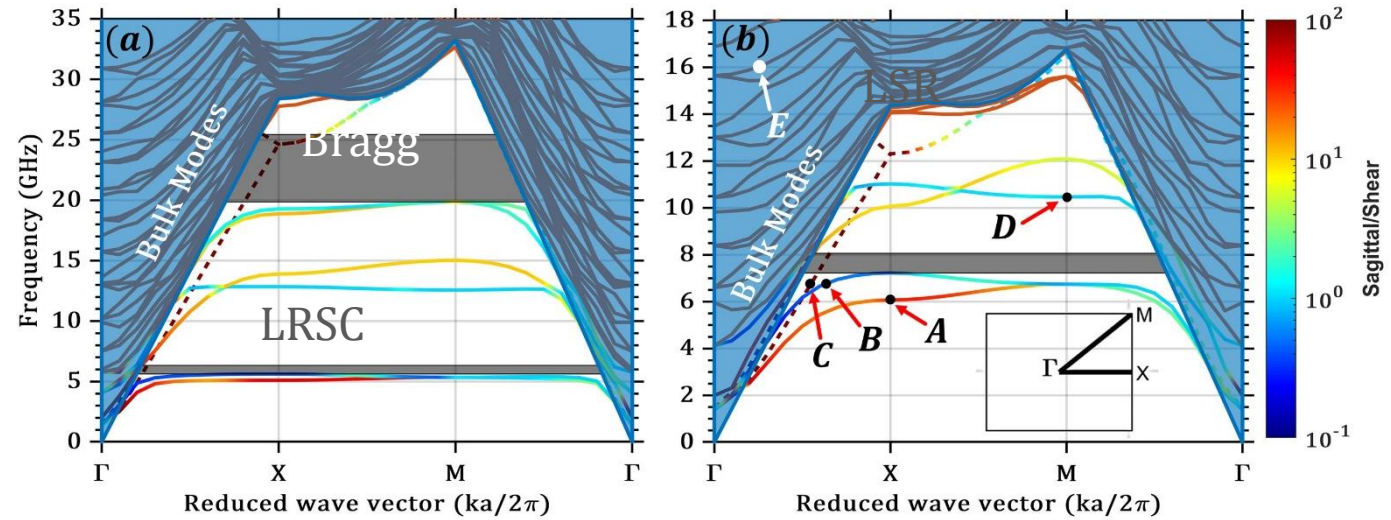
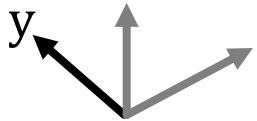
Pillar-Based PnC



Sagittal polarization:

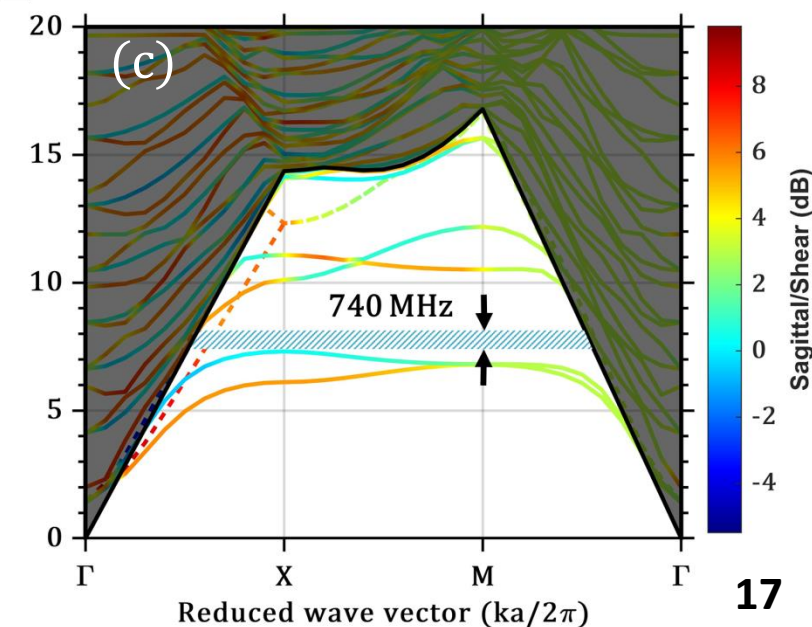
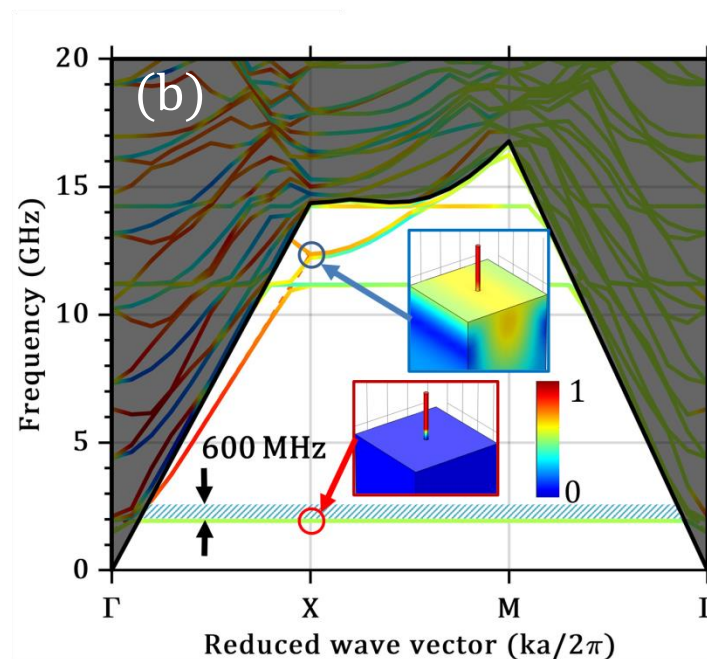
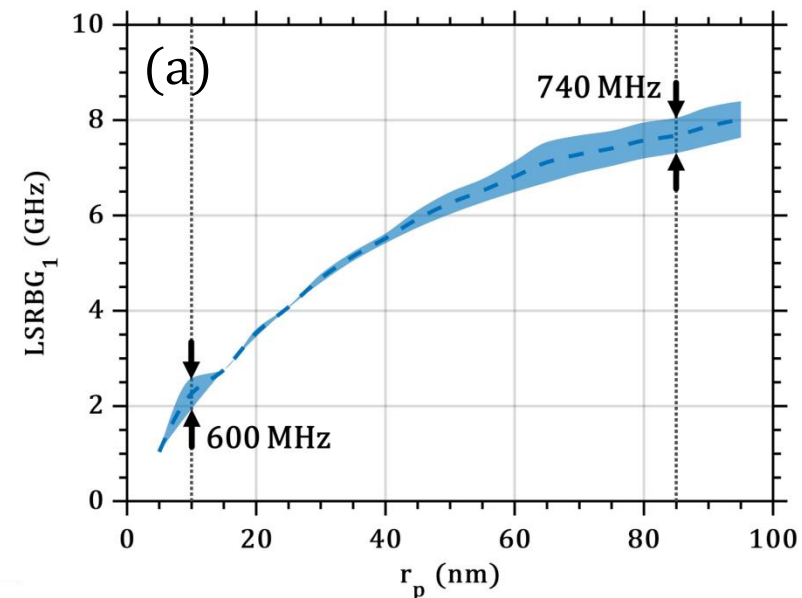
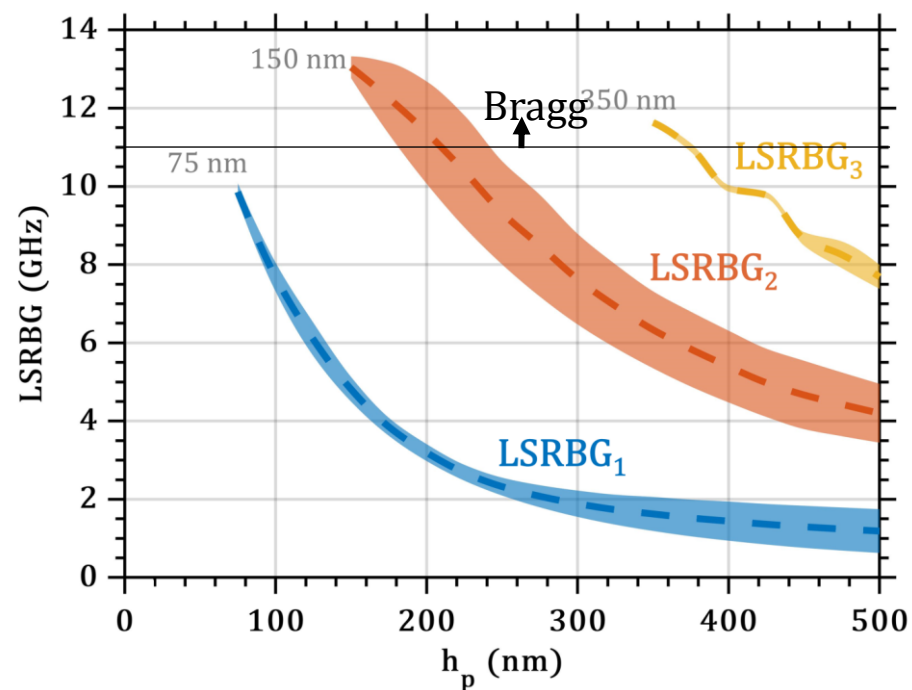
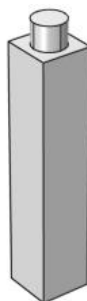


Shear polarization:

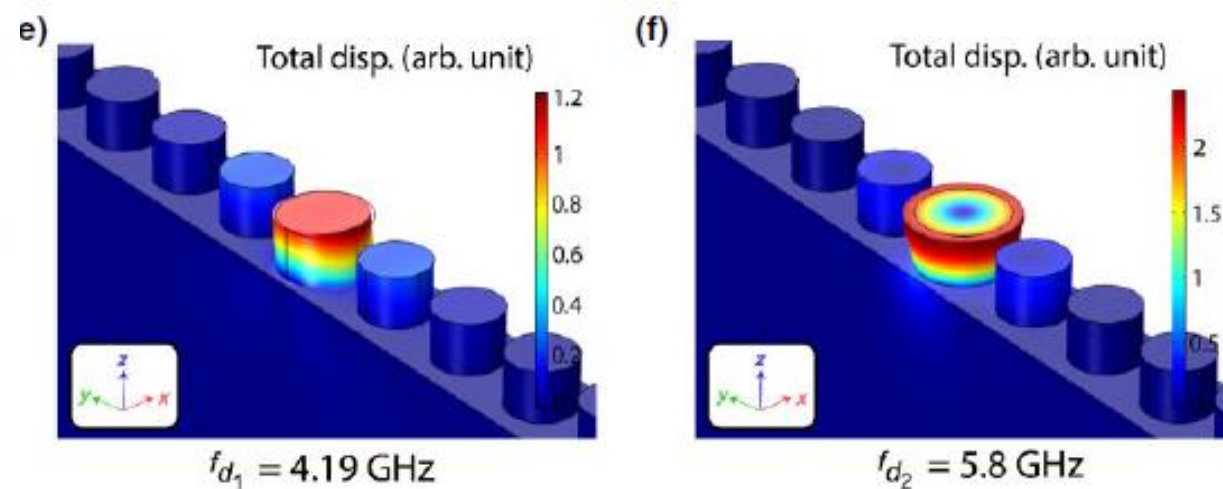
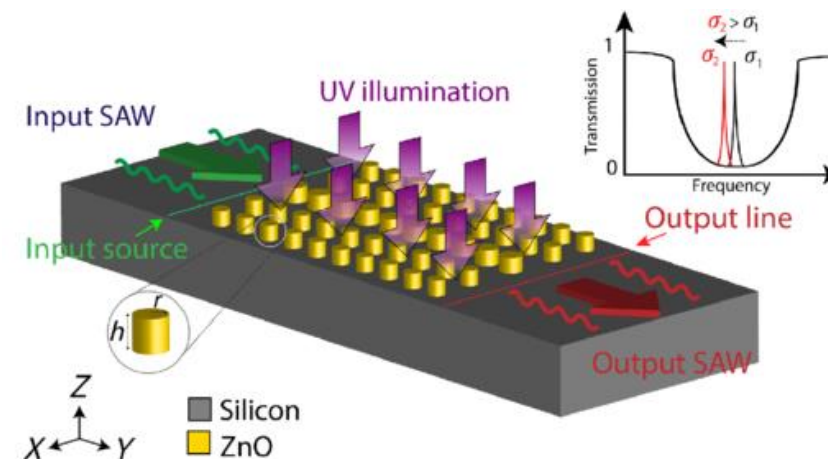
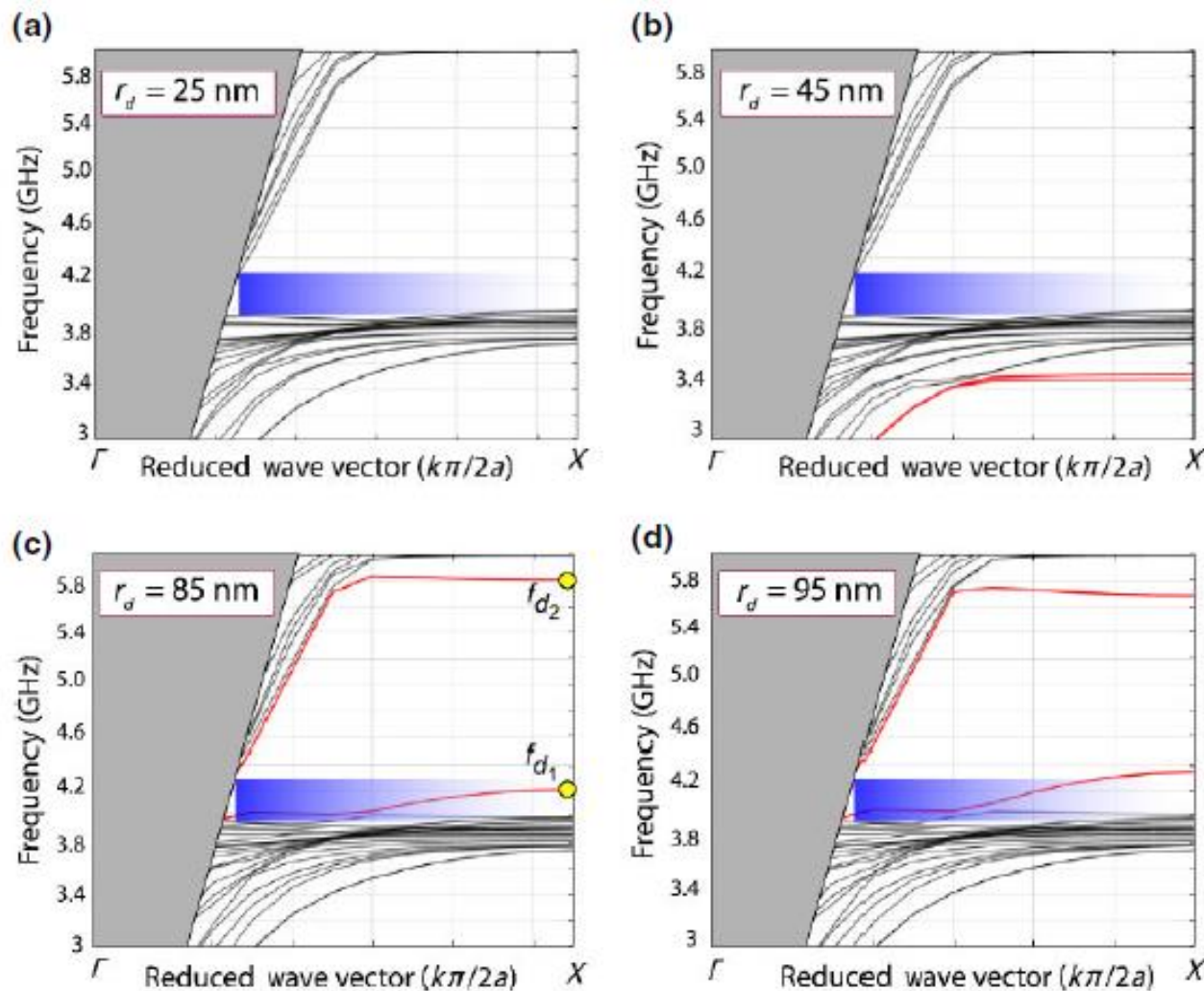


Pillar-Based PnC

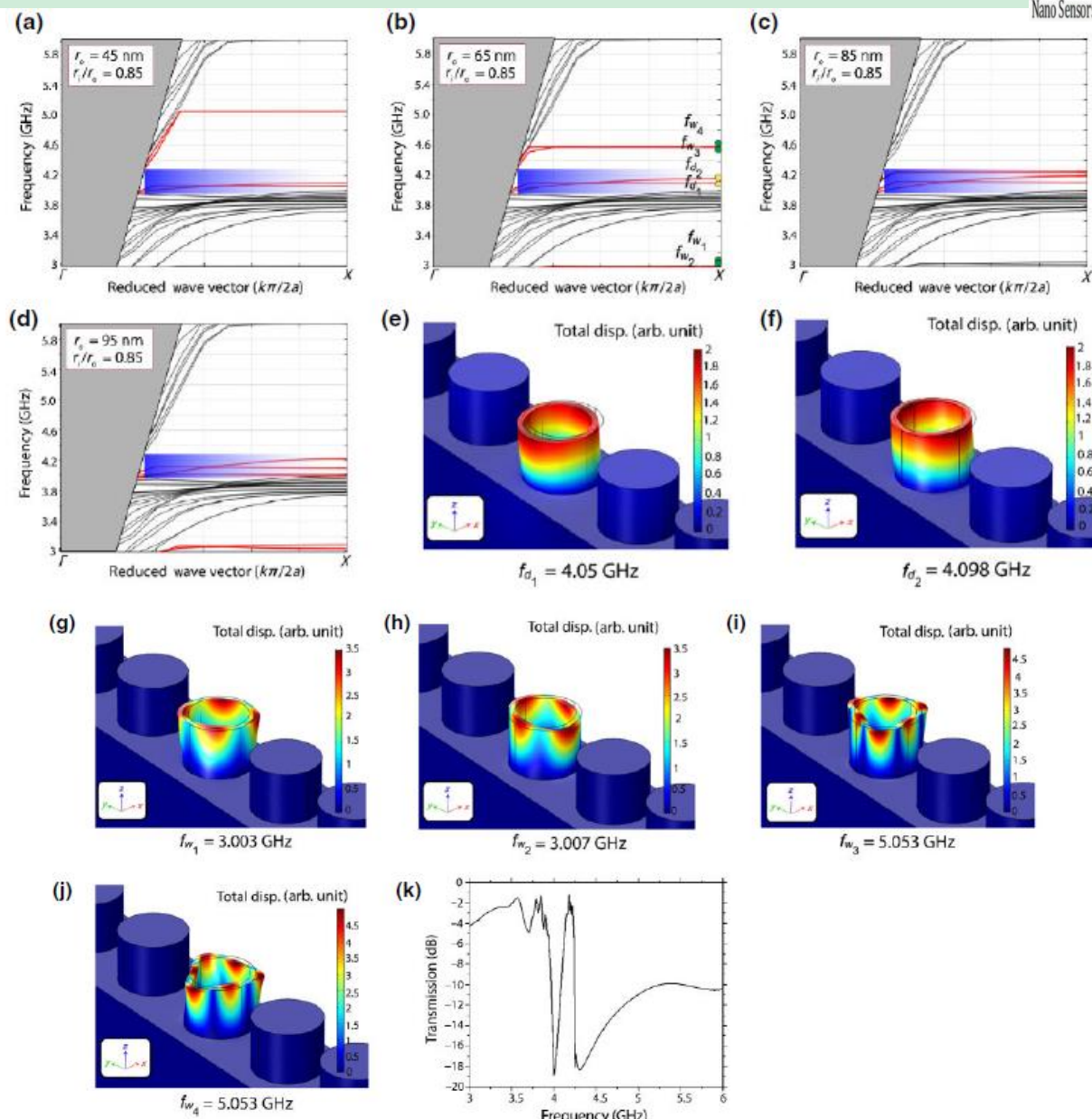
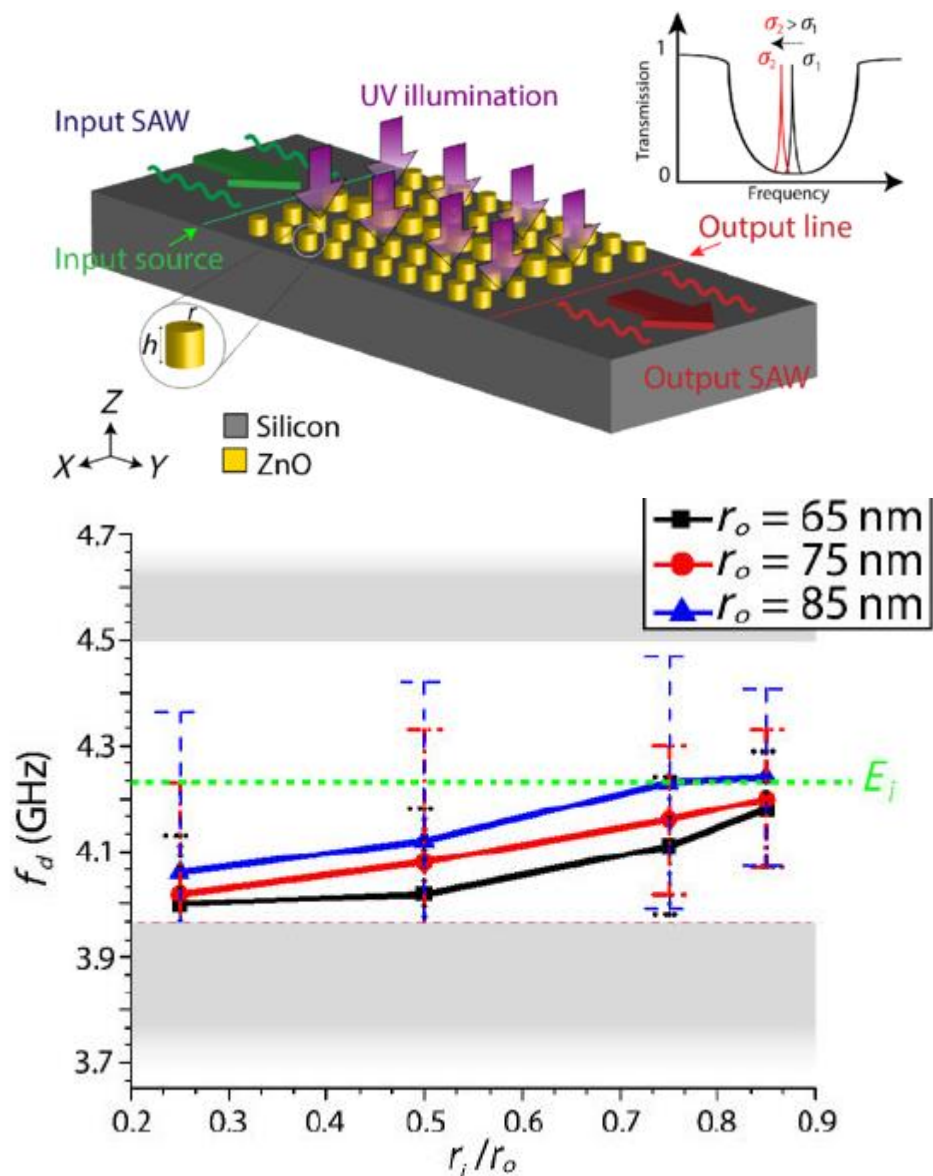
LRSC Bandgap Central Frequency



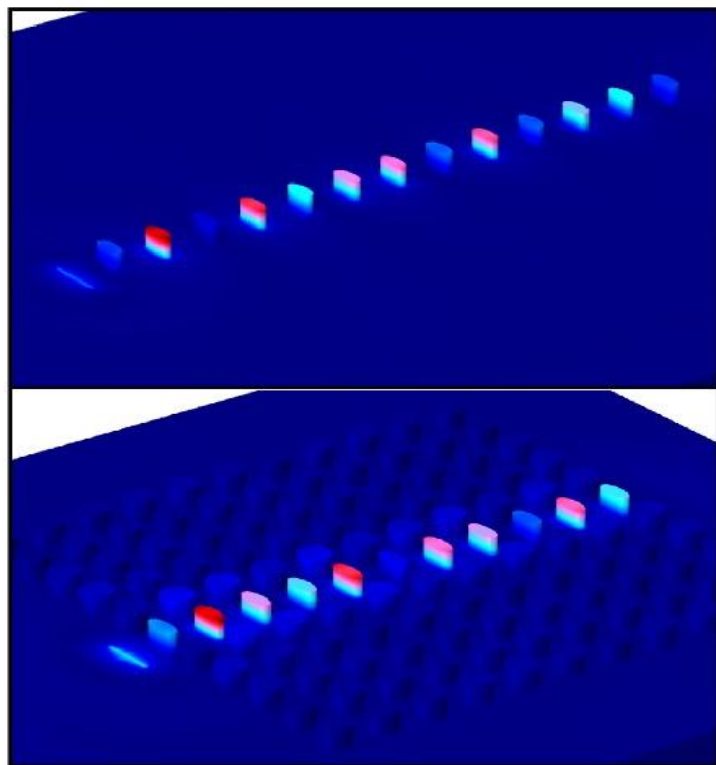
Localized LRSC Modes in defects



Localized LRSC Modes in defects

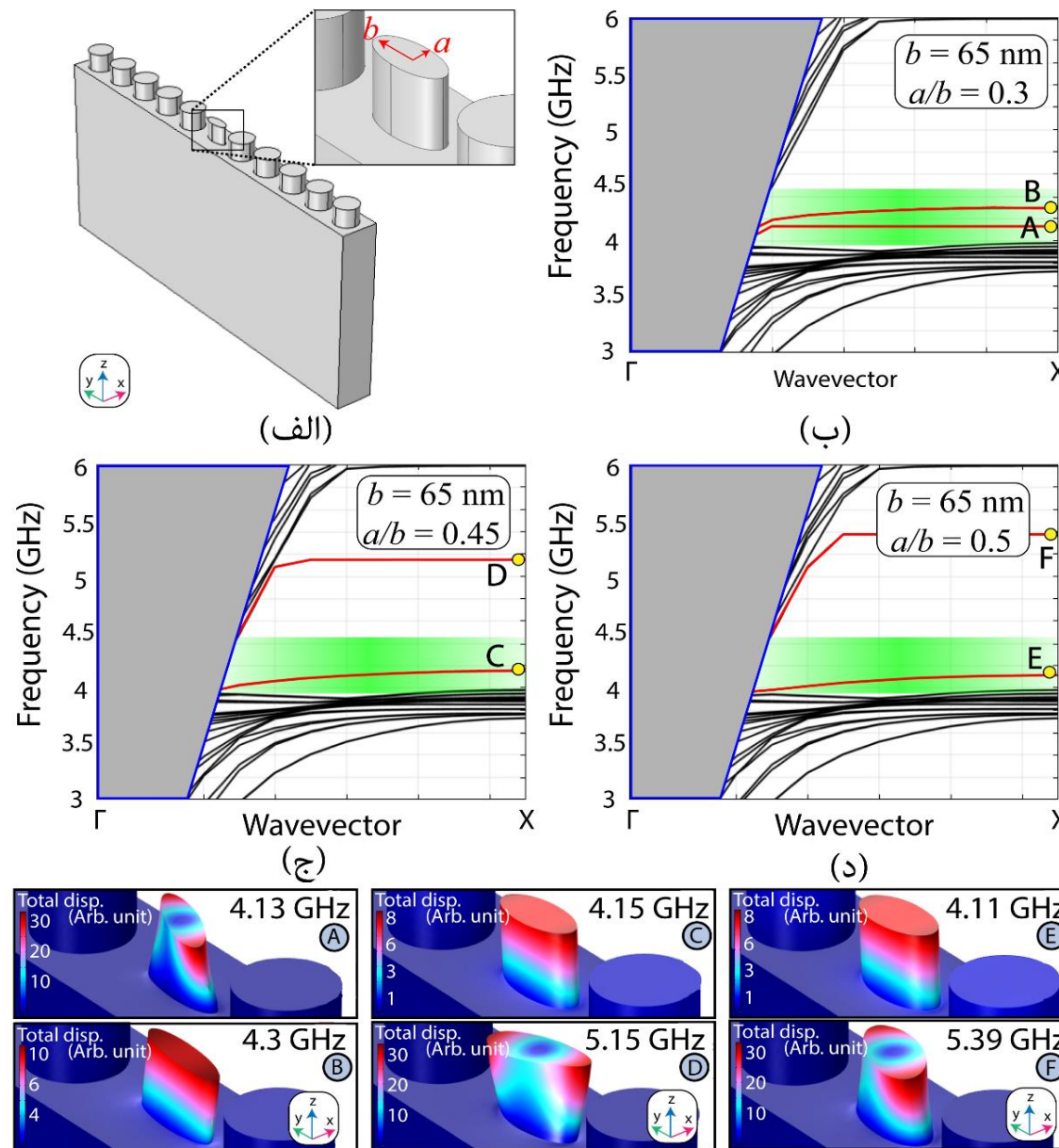


Localized LRSC Modes in defects



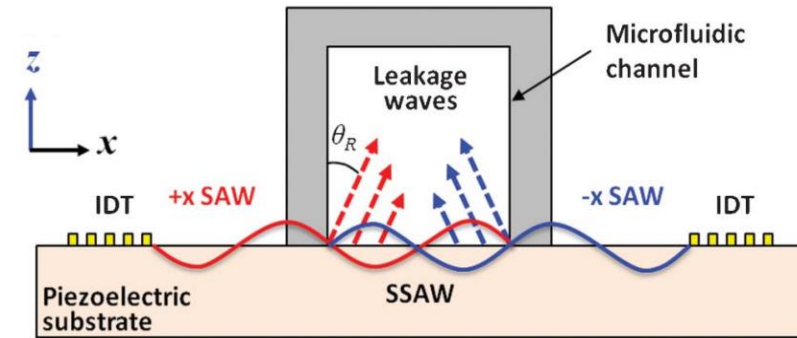
$$f_d = 4.2 \text{ GHz}$$

Taleb, et al. *Journal of Physics D: Appl. Phys.* 2021.



Governing equations in the fluid:

- $p = p(\rho)$
- Continuity equation : $\partial_t \rho = -\nabla \cdot (\rho v)$
- Navier-stokes equation : $\rho \partial_t v = -\nabla p - \rho(v \cdot \nabla)v + \eta \nabla^2 v + \beta \eta \nabla(\nabla \cdot v)$



X. Ding, *Lab Chip*, 2013

Fluid pressure, velocity and density, up to second order of perturbation:

- $p = p_0 + p_1 + p_2 + \dots$
- $v = v_0 + v_1 + v_2 + \dots$
- $\rho = \rho_0 + \rho_1 + \rho_2 + \dots$

First- and Second-Order of Acoustic Fields

First-order fields:

$$p_1 = \rho_1 c_f^2$$

$$\triangleright \nabla^2 p_1 = \frac{1}{c_f^2} \partial_t^2 p_1, \eta = 0$$

$$\triangleright \rho_0 \partial_t v_1 = -c_f^2 \nabla \rho_1 = \nabla p_1$$

$$\triangleright \partial_t \rho_1 = -\rho_0 (\nabla \cdot v_1)$$

Second-Order fields:

$$\triangleright \rho_0 \nabla \cdot \langle v_2 \rangle = -\nabla \cdot \langle \rho_1 v_1 \rangle$$

$$\triangleright \nabla \langle p_2 \rangle = -\langle \rho_1 \partial_t v_1 \rangle - \langle \rho_0 (v_1 \cdot \nabla) v_1 \rangle$$

Acoustic Forces in Acoustofluidics

Motion of Particle:

$$m_p \frac{dv_p}{dt} = F_{rad} + F_{drag}$$



Nguyen et al., *Appl. Phys. Lett.*, 2018

Acoustic Radiation Force:

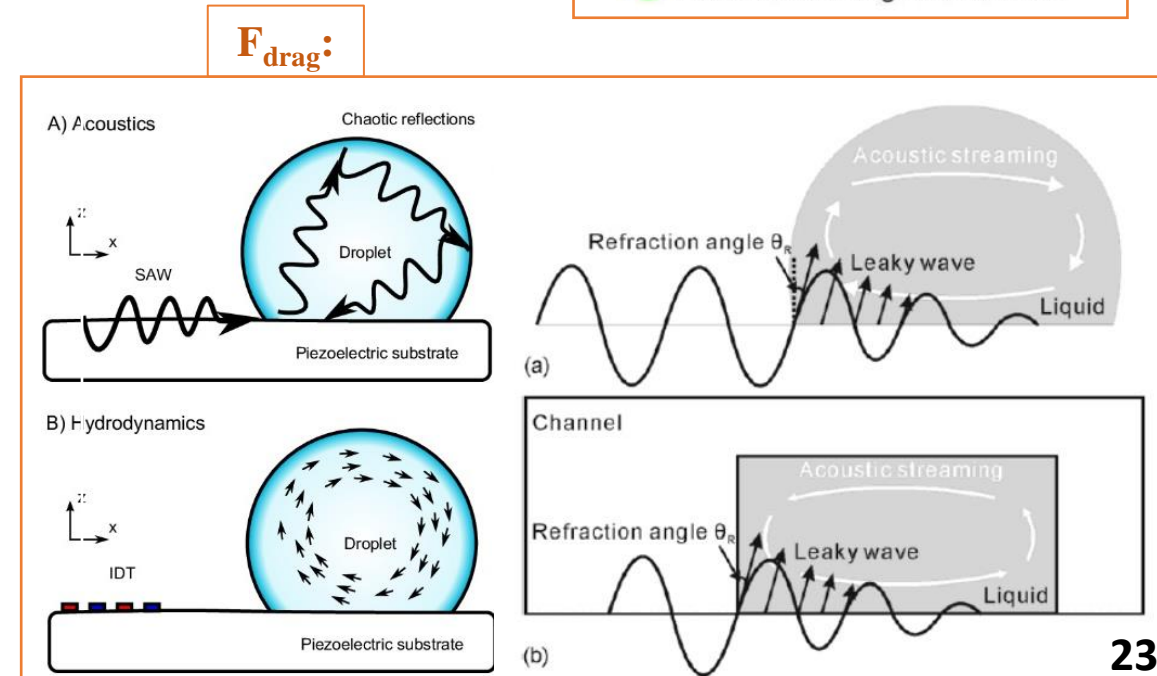
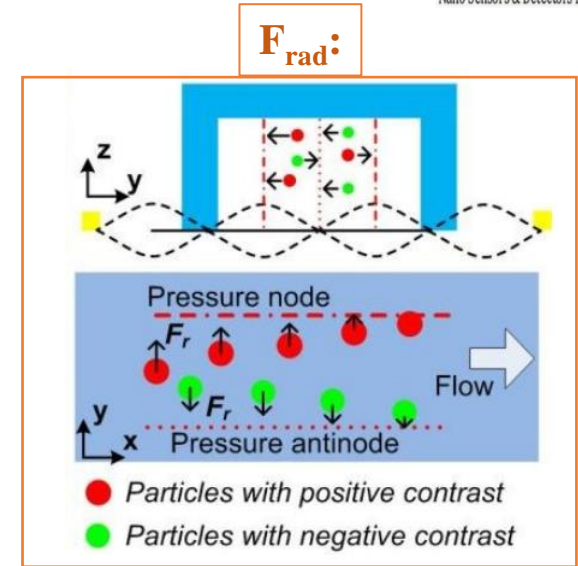
$$F_{rad} = -\nabla U_{rad} = \frac{-4\pi}{3} R^3 \nabla [f_1 \frac{1}{2\rho_0 c_f^2} \langle p^2 \rangle - f_2 \frac{3}{4} \rho_0 \langle v^2 \rangle]$$

$$f_1 = 1 - \frac{k_p}{k_f}, \quad f_2 = \frac{2(\frac{\rho_p}{\rho_f} - 1)}{2(\frac{\rho_p}{\rho_f} + 1)}$$

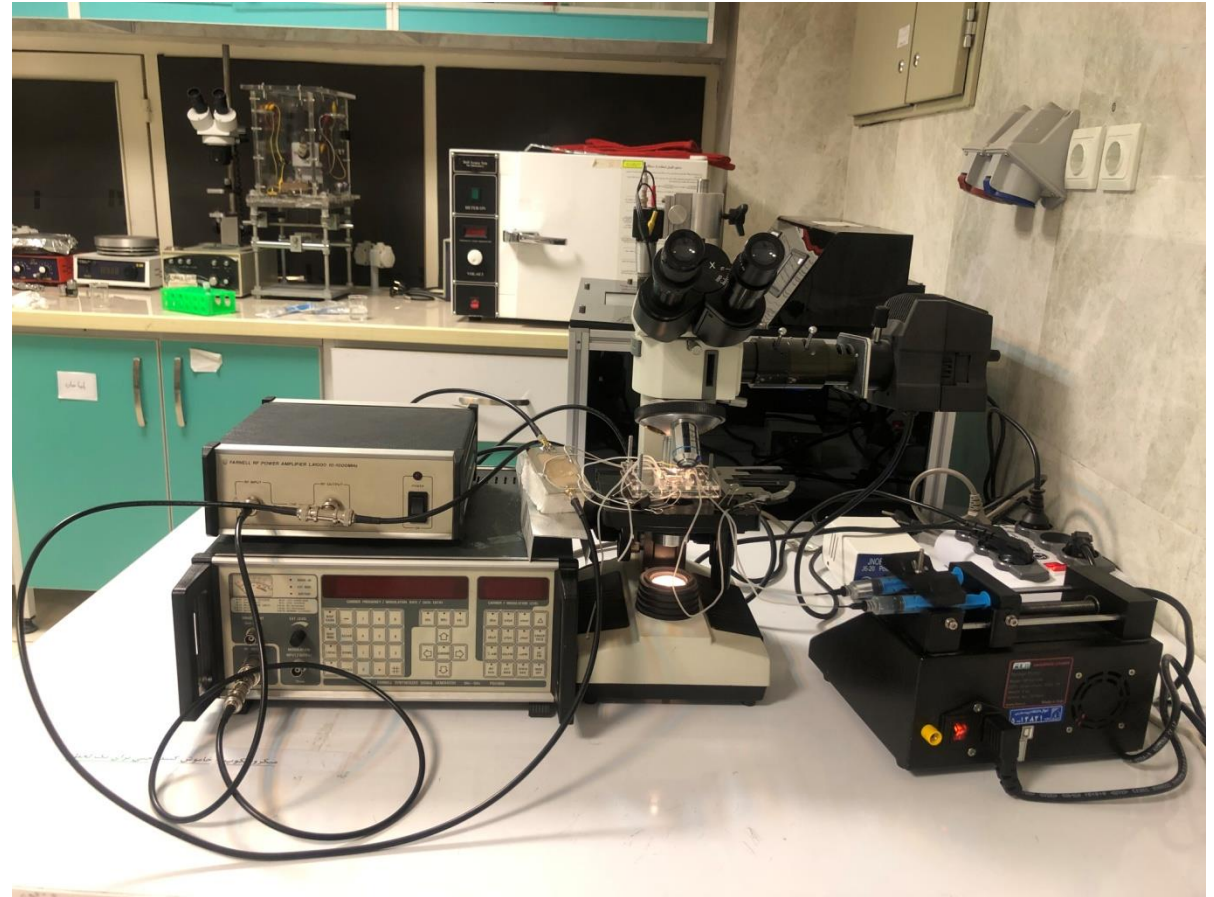
Acoustic Induced Drag Force:

- $F_{drag} = 6\pi R\eta(\langle v_2 \rangle - v_p)$

H. Bruus, *Lab Chip*, 2012



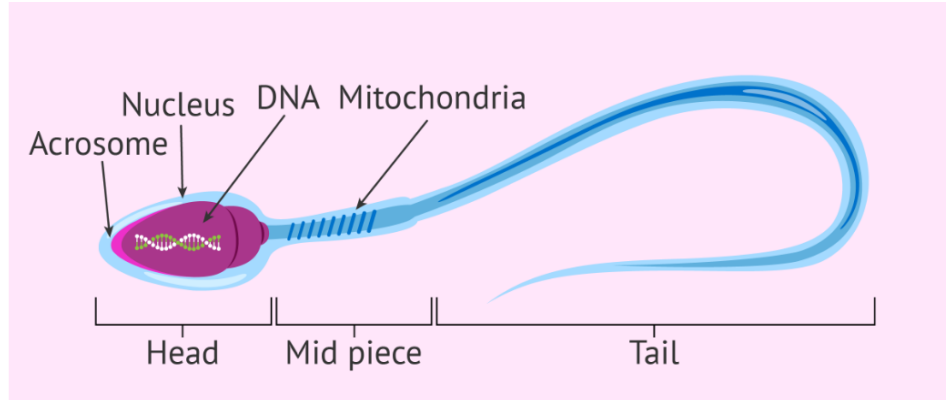
Acoustofluidics based on LRSCMs in SU-8 Ridges



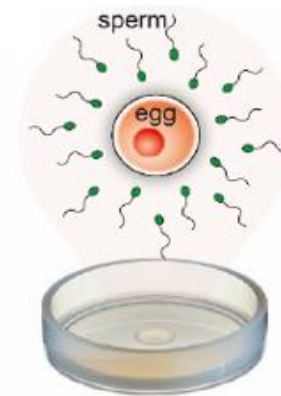
LiNbO₃-based Acoustofluidics

SAW-in-capillary for separating highly motile sperm cells

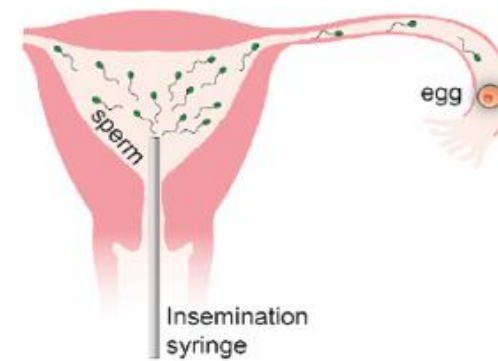
- ❖ The structure of human sperm consisting of a head and a flagellum
- ❖ Assisted reproductive technologies



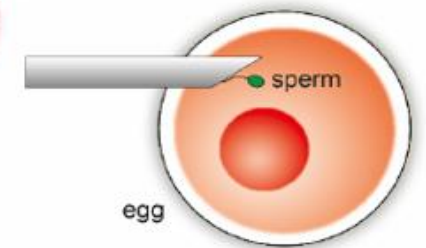
Structure and parts of a sperm cell



a) IVF



b) IUI



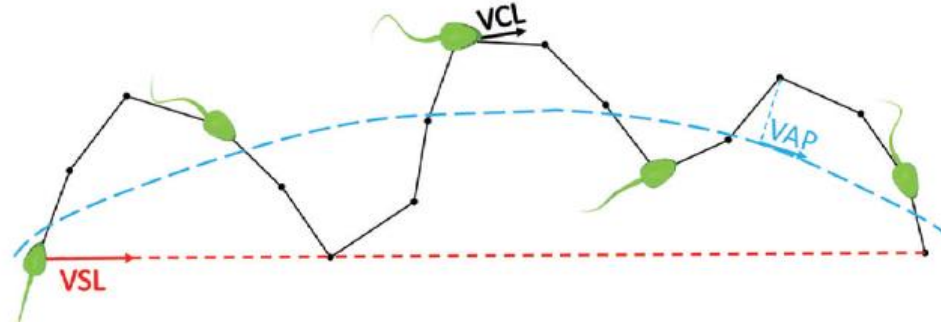
c) ICSI

Assisted reproductive technologies a) In vitro fertilization b) Intrauterine Insemination c) Intracytoplasmic sperm injection

SAW-in-capillary for separating highly motile sperm cells

❖ Important parameters of sperm:

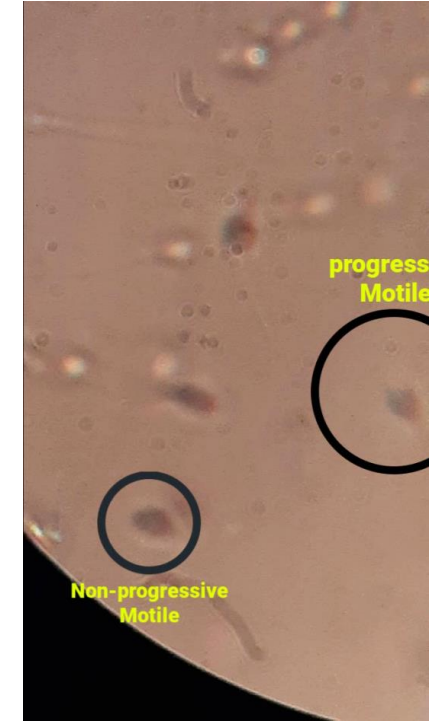
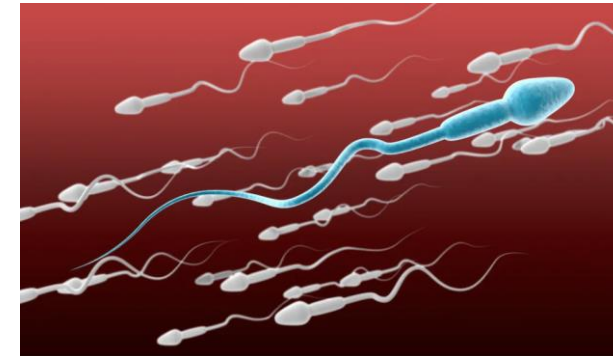
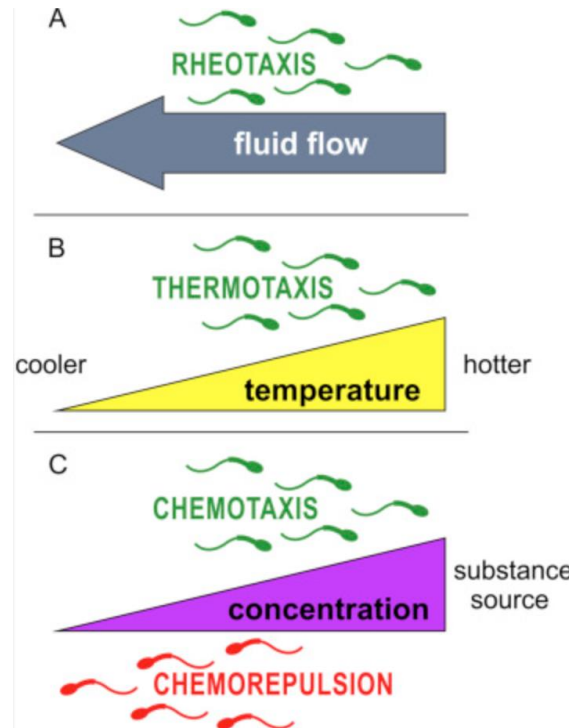
- ❖ Motility
- ❖ Vitality



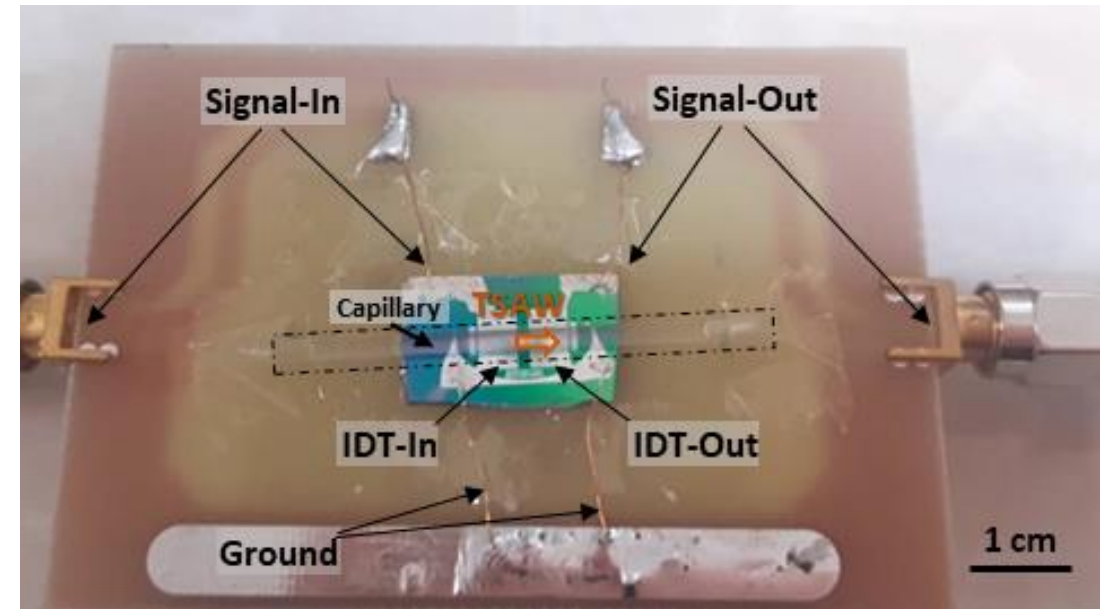
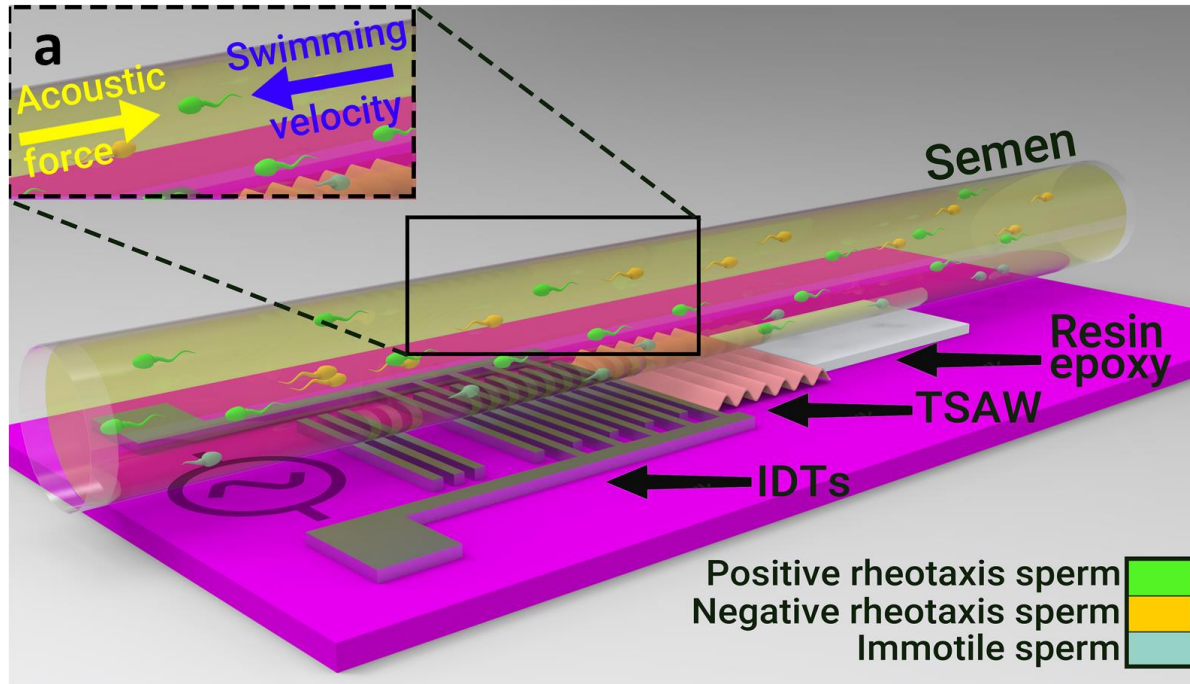
visual representation of kinematic velocities of sperm

❖ Sperm natural behavior:

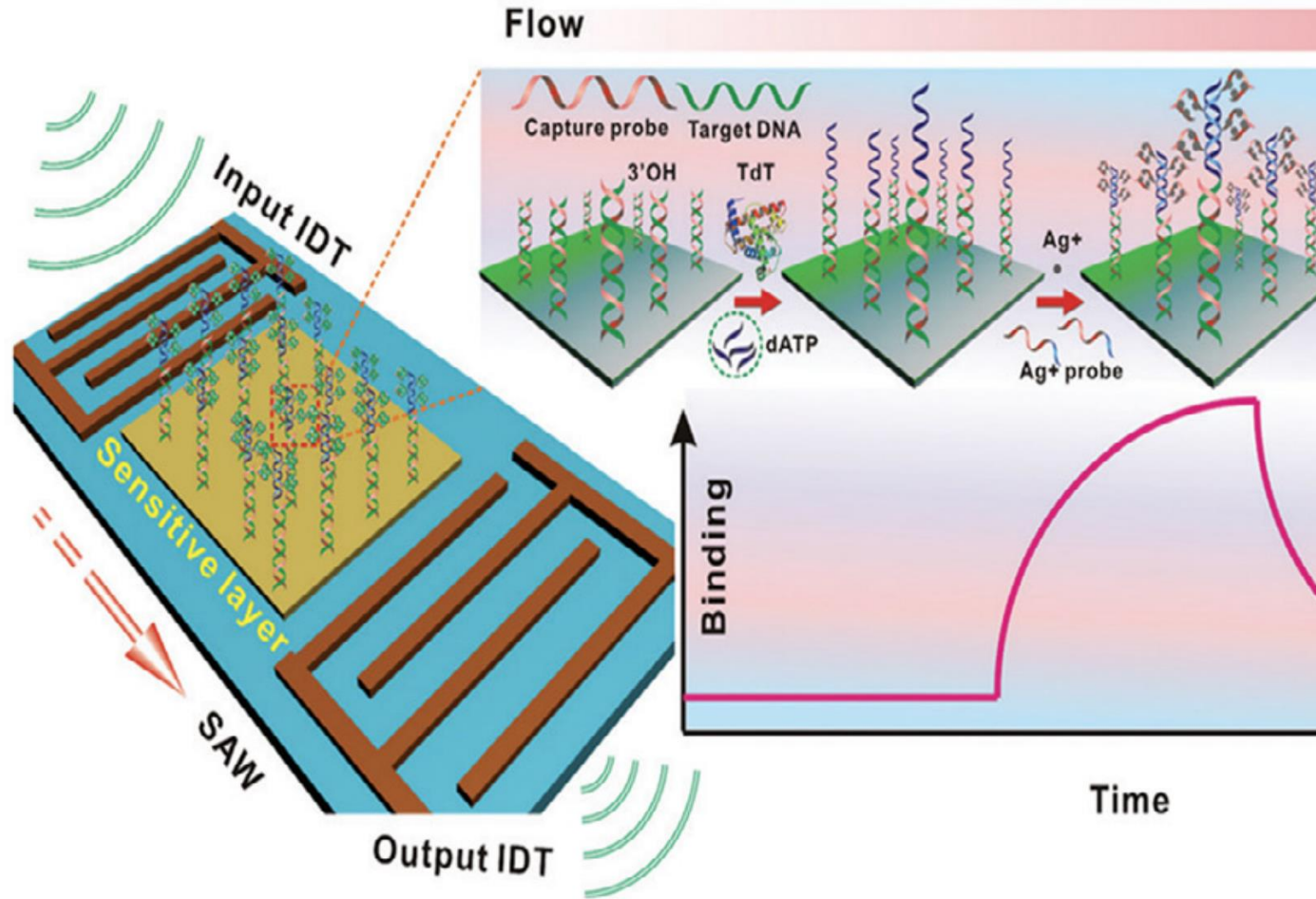
- ❖ Rheotaxis
- ❖ Thermotaxis
- ❖ Chemotaxis
- ❖ Acoustotaxis



SAW-in-capillary for separating highly motile sperm cells

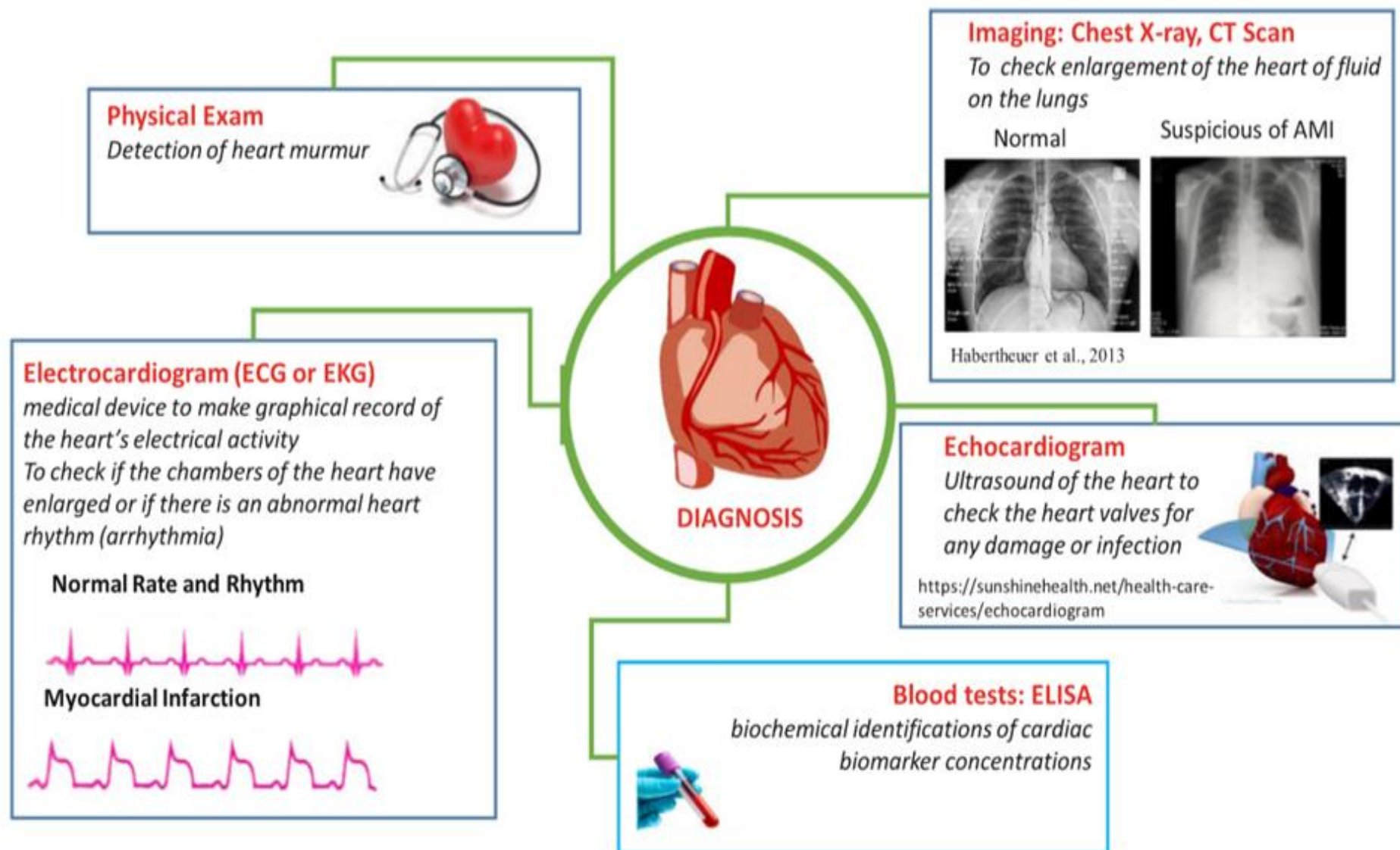


SAW-based Biosensors

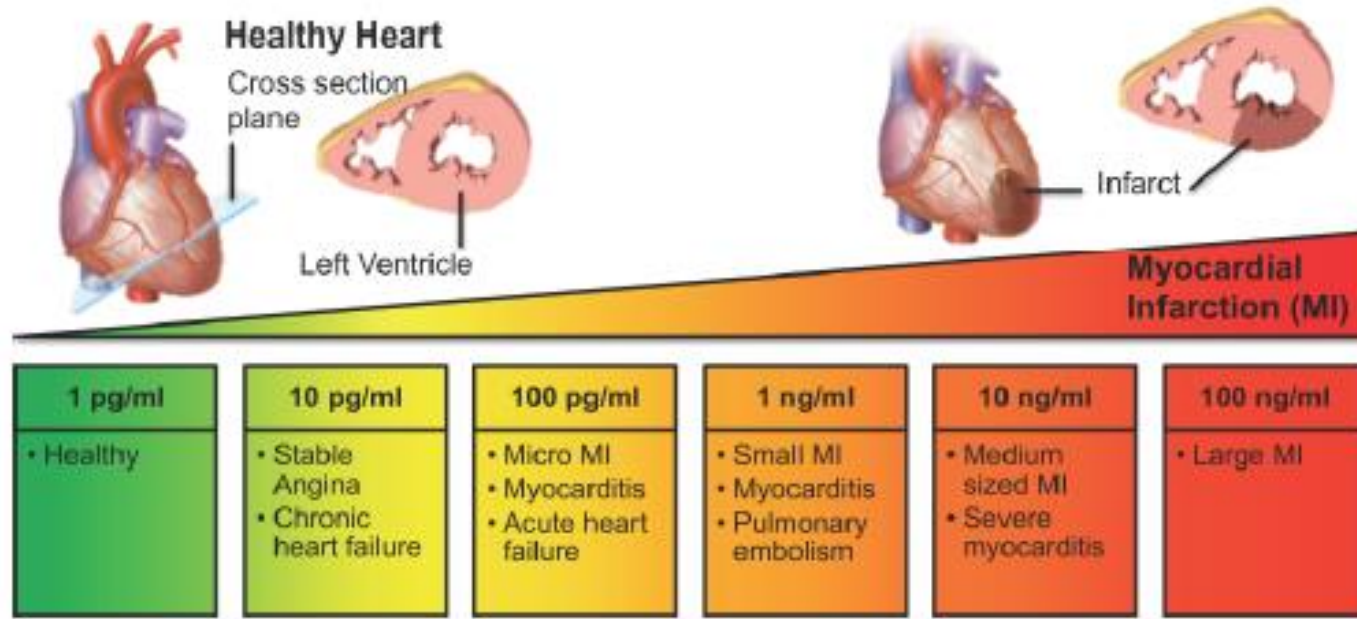


Y. Zhang et al., *Analyst* 2017

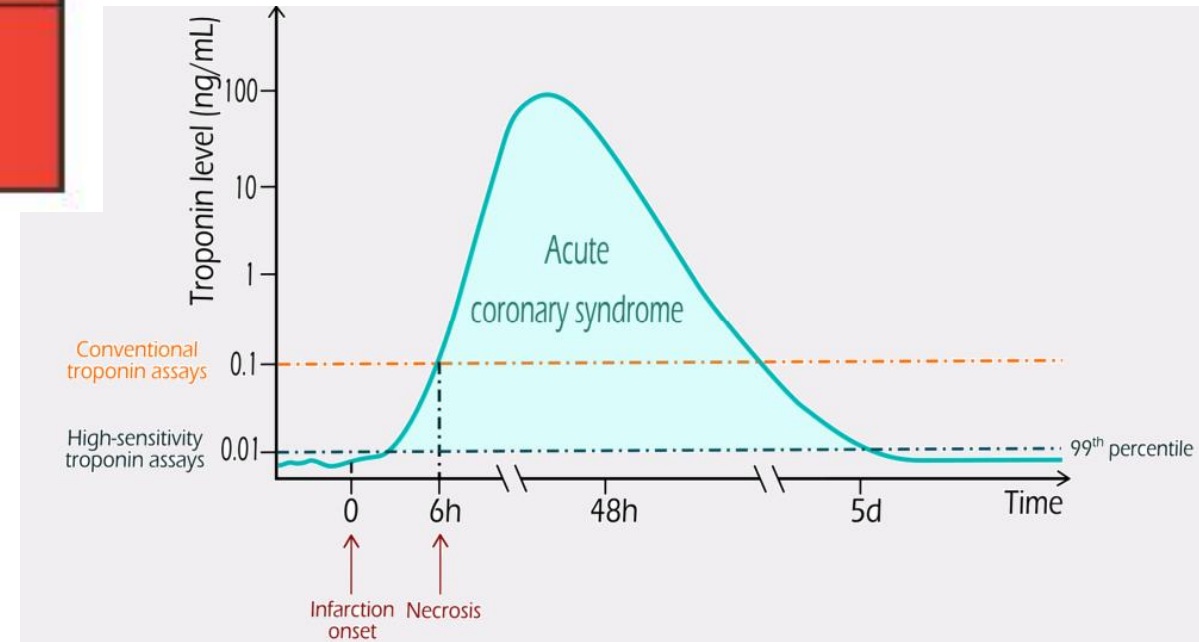
SAW-Biosensor for Detection of Cardiac Troponin I



SAW-Biosensor for the Detection of Cardiac Troponin I

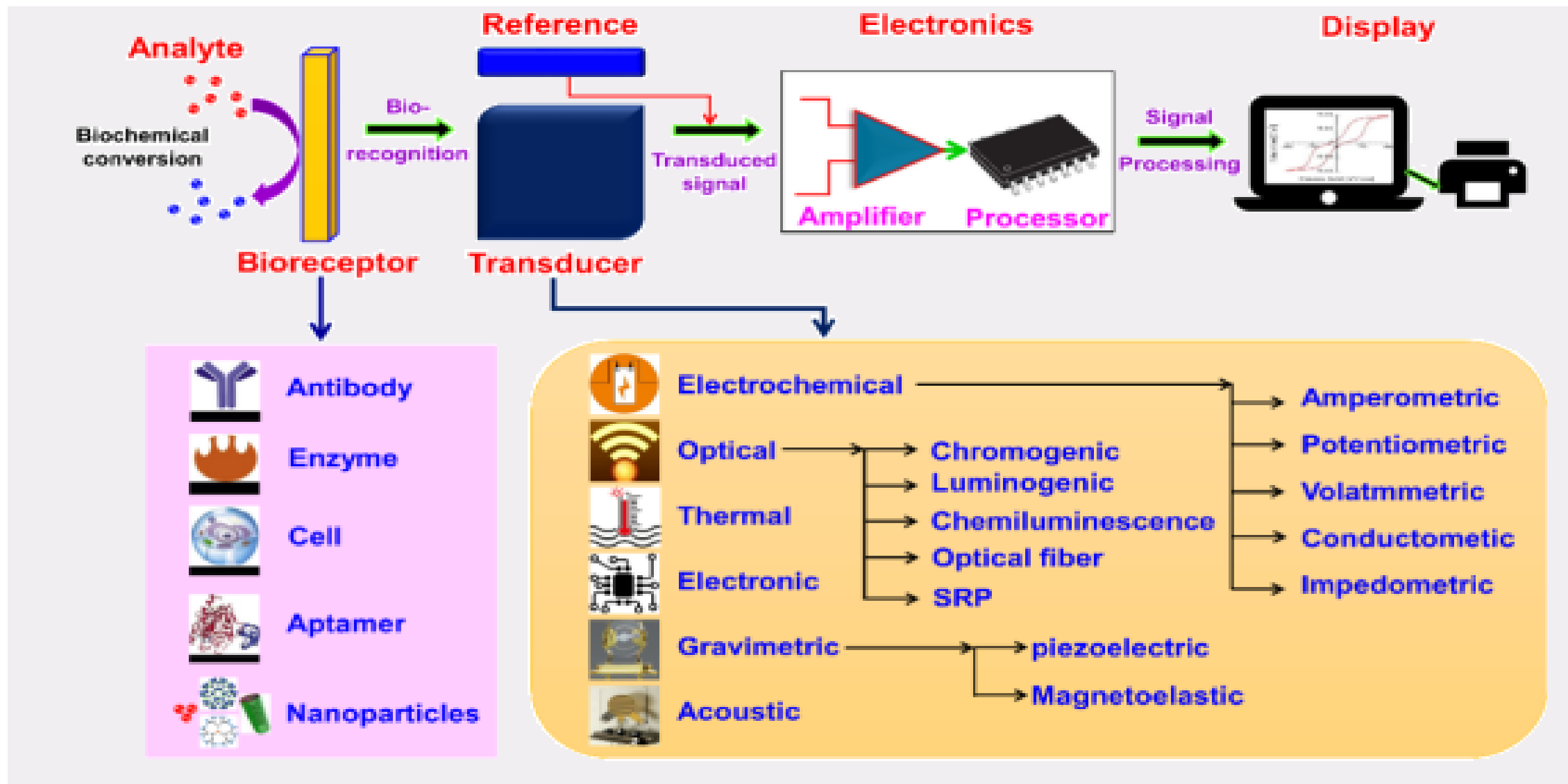


cTnI in healthy humans: lower than 0.04 ng mL^{-1}
 increased risk for acute heart failure: around 0.1 ng mL^{-1}



M. Savonnet.et al., *Pharmaceutical and Biomedical Analysis*, 2020

SAW-Biosensor for the Detection of Cardiac Troponin I



SAW-Biosensor for the Detection of Cardiac Troponin I

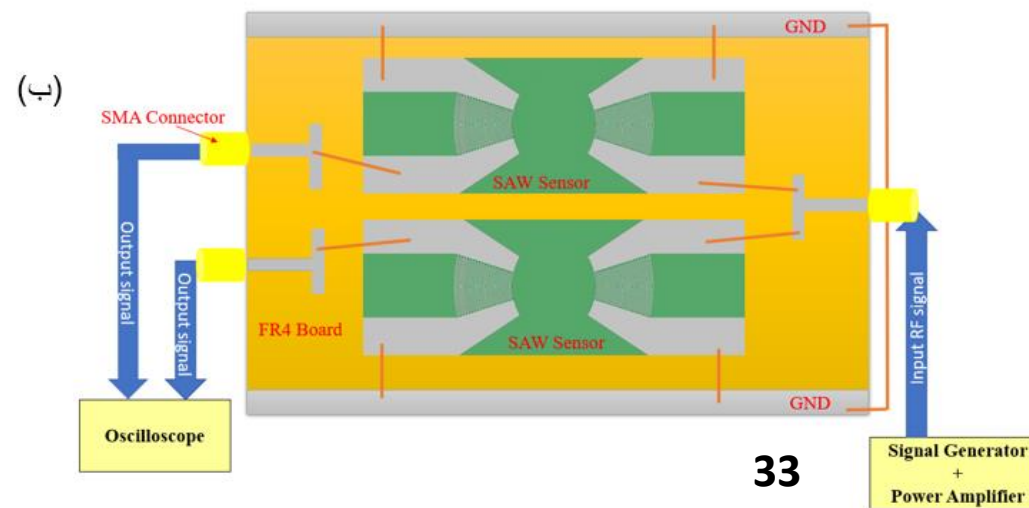
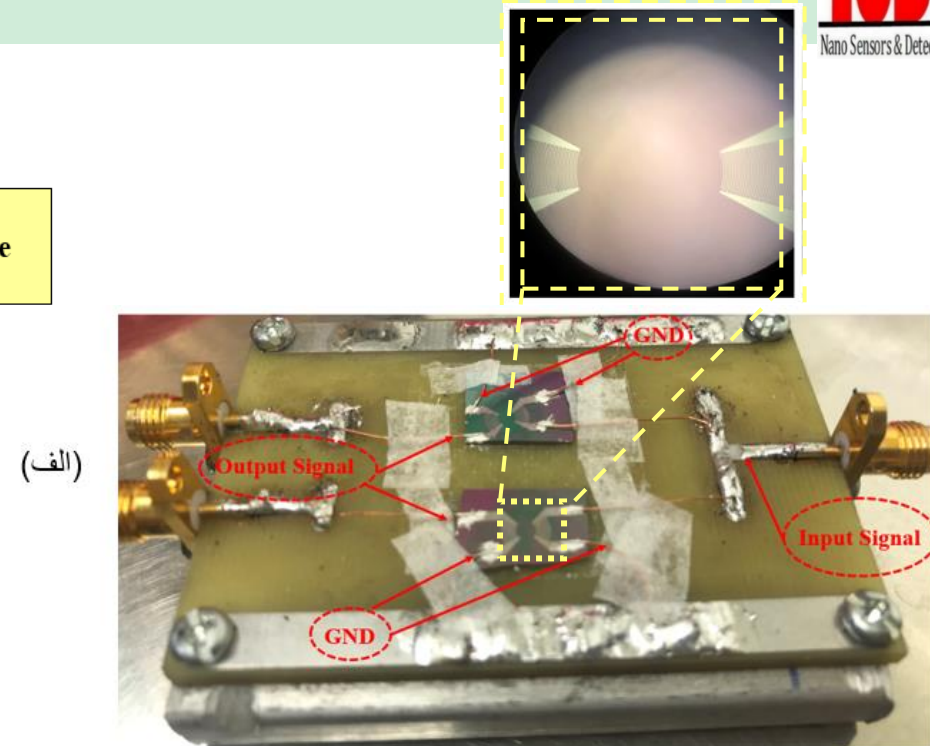
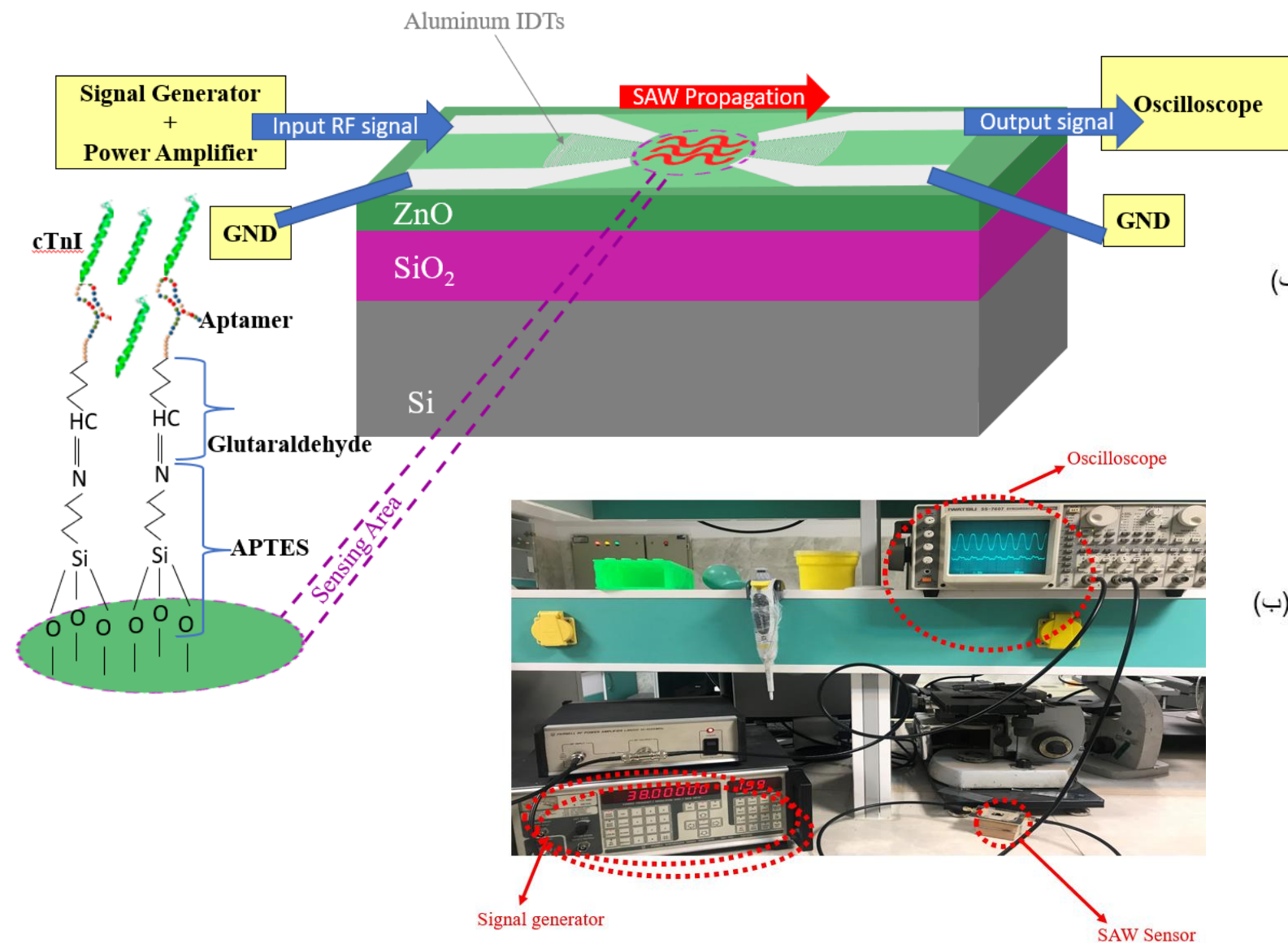
Features	Antibody	Aptamer
Specificity	High	High
Size	Relatively high	Small
Stability	Unstable	Stable
Affinity	High	High
Immunogenicity	High	No humoral response
Potential target	Immunogenic molecules	Any target
Production	In vivo	In vitro
Cost	Expensive	Relatively cheap
Modification	Limited	Almost unlimited
Time to generate	~6 months	~3–7 weeks
Renal separation	Slow	Fast

V. Subjakova.et al., *Polymers* 13, 2021

Sequence (5' to 3')	K _d value (cTnI)	K _d value (Troponin complex)
TCACACCCTCCCTCCCA CATACCGCATACACTTTT TGATT	3.41 nM	3.12 nM
CCCGACCACGTCCCTGTC CCTTTCCTAACCTGTTT GTTGAT	1.13 nM	4.47 nM
ATGCGTTGAACCTCCT GACCGTTTATCACATACT CCAGA	1.14 nM	5.70 nM
CGTGCAGTACGCCAACC TTTCTCATGCGCTGCC CTCTTA	270 pM	3.10 nM
CAACTGTAATGTACCCTC CTCGATCACGCACCACT TGCAT	3.25 nM	10.61 nM
CGCATGCCAACGTTGC CTCATAGTTCCCTCCCC GTGTCC	317 pM	3.37 nM

H. Jo.et al., *Analytical chemistry*, 2015

SAW-Biosensor for the Detection of Cardiac Troponin I



Conclusion

The Proposed tweezers based on SAWs are promising for:

- Application in efficient and compact Lab-on-Chip systems
- Realizing locally reinforced particle manipulation
- Manipulation of sub-wavelength small particles
- Label-free manipulation of target particles
- High potential for novel and enhanced functionalities by introducing metasurfaces in the active zone of the channel.

Special Thanks to Bio-Acoustics group members

Farzaneh Soleimani

Pouya Khorshidian

Mehran Azadbakht

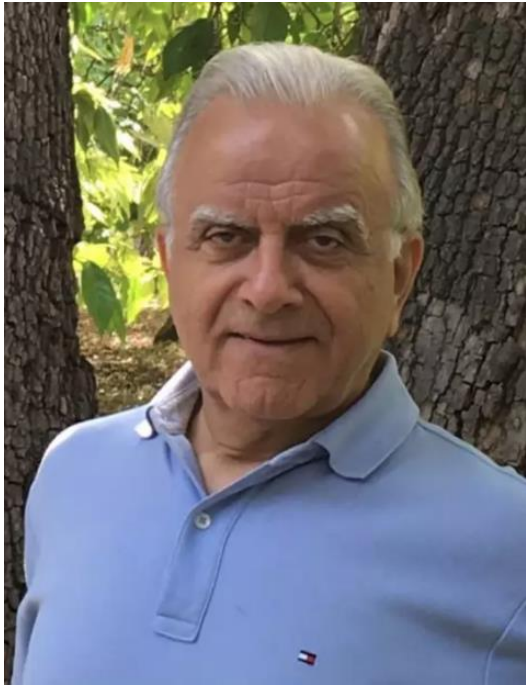
Behdad Barahimi

Hourieh Ebrahimi

Sara Abbasi



Thanks to my Bio-Acoustics Academic collaborators



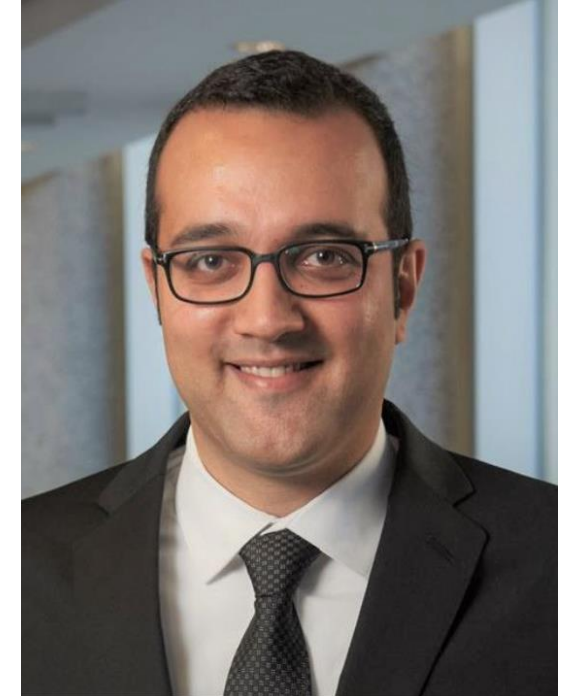
Dr. Mohammad-Kazem Moravvej,
Faculty of Electrical and
Computer Engineering, TMU,
Iran



Dr. Mohammad Zabetian,
Faculty of Mechanical
Engineering, TMU, Iran



Dr. Iman Halvaei
Faculty of Medical Sciences,
TMU, Iran



Dr. Reza Nosrati
Department of Mechanical
Engineering, Monash University,
Austria

Thanks for your attention

